

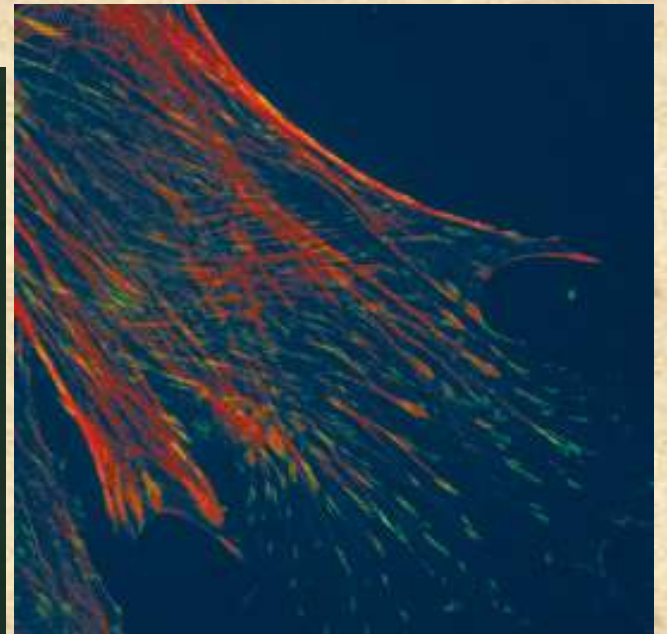
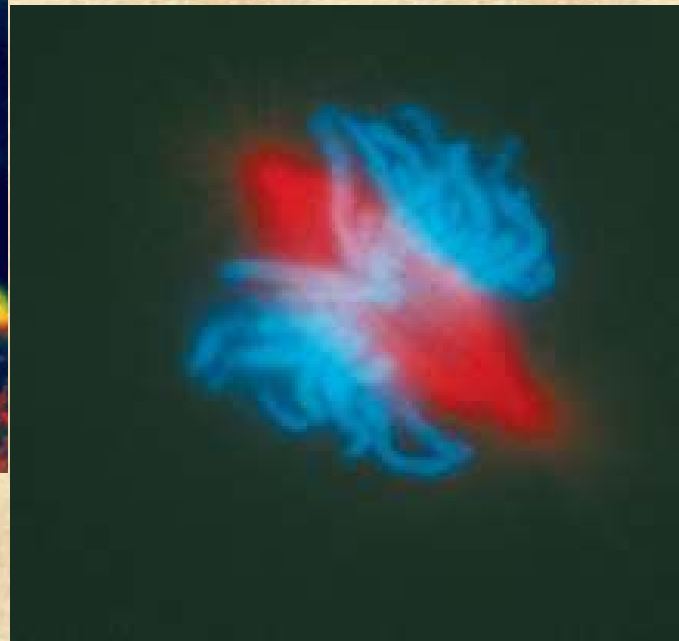
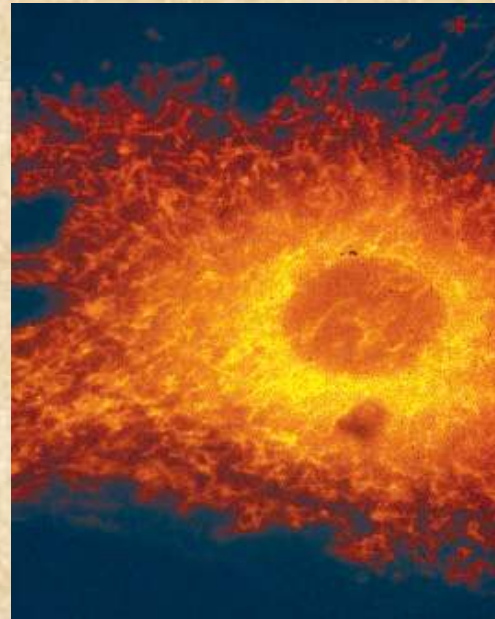
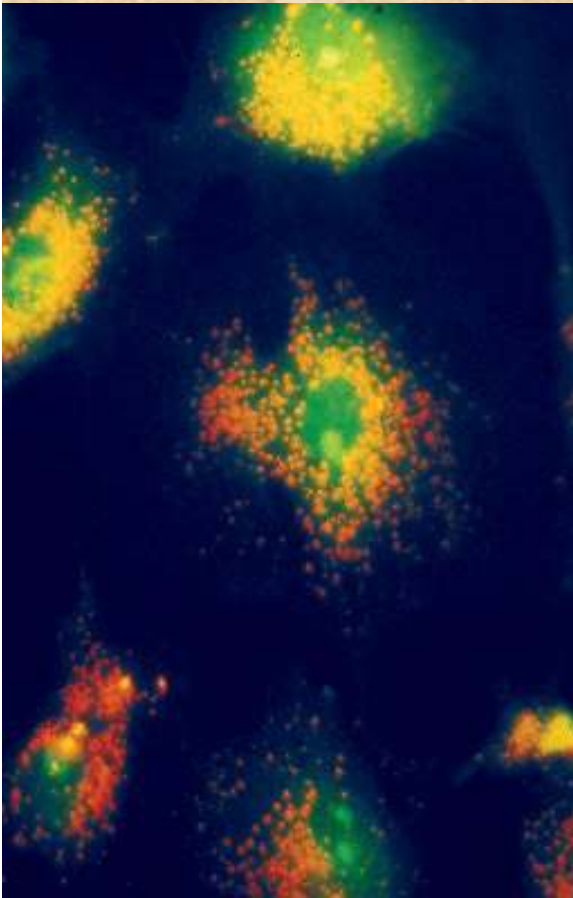
Prof. Enrico Gratton - Lecture 6

Fluorescence Microscopy

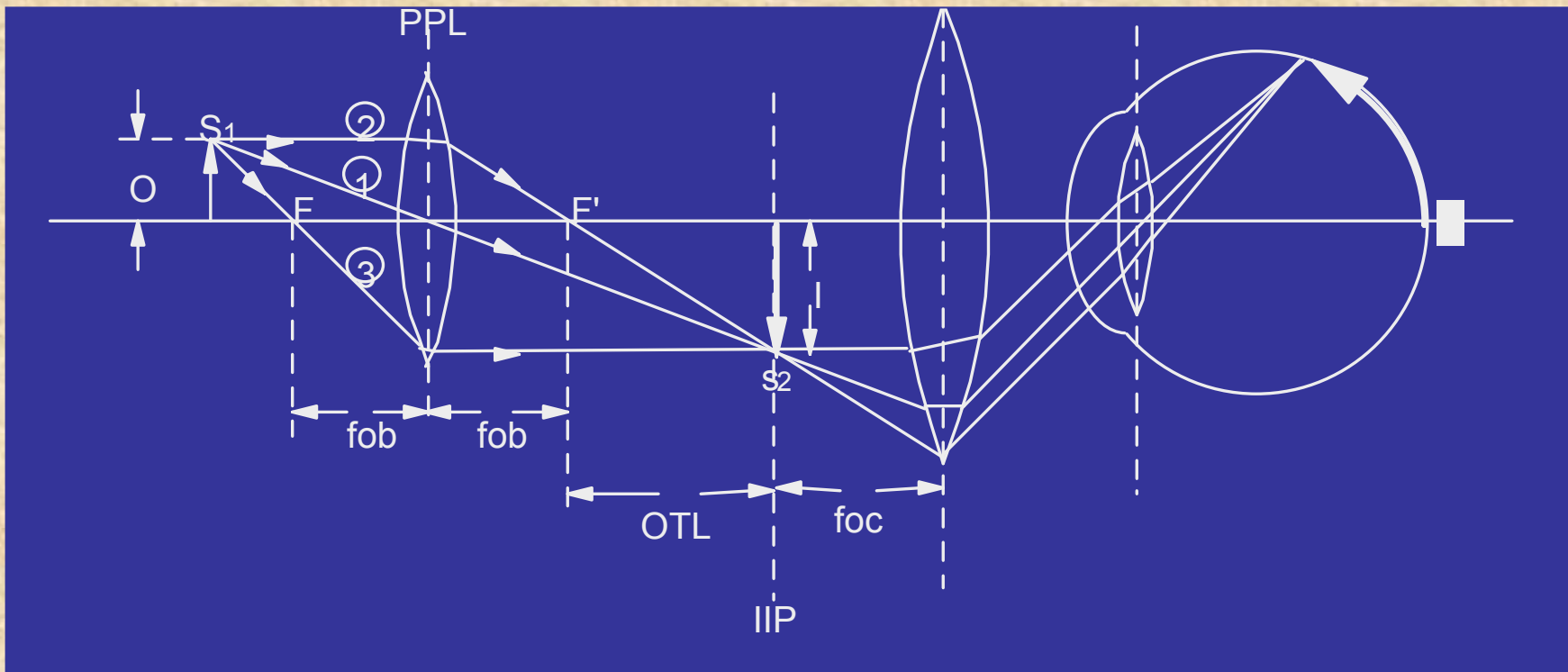
Instrumentation
Light Sources:
One-photon and Multi-photon Excitation
Applications in Cells
Lifetime Imaging

Figures acknowledgements: E.D. Salmon and K. Jacobson

Confocal microscopy images



In the compound microscope the Finite Corrected Objective Forms a Real Image At the Ocular Front Focal Plane: The Primary or Intermediate Image Plane (IIP)



Conventional Optics

Objective with finite Focal Length

(Optical Tube Length, OTL, Typically 160 mm)

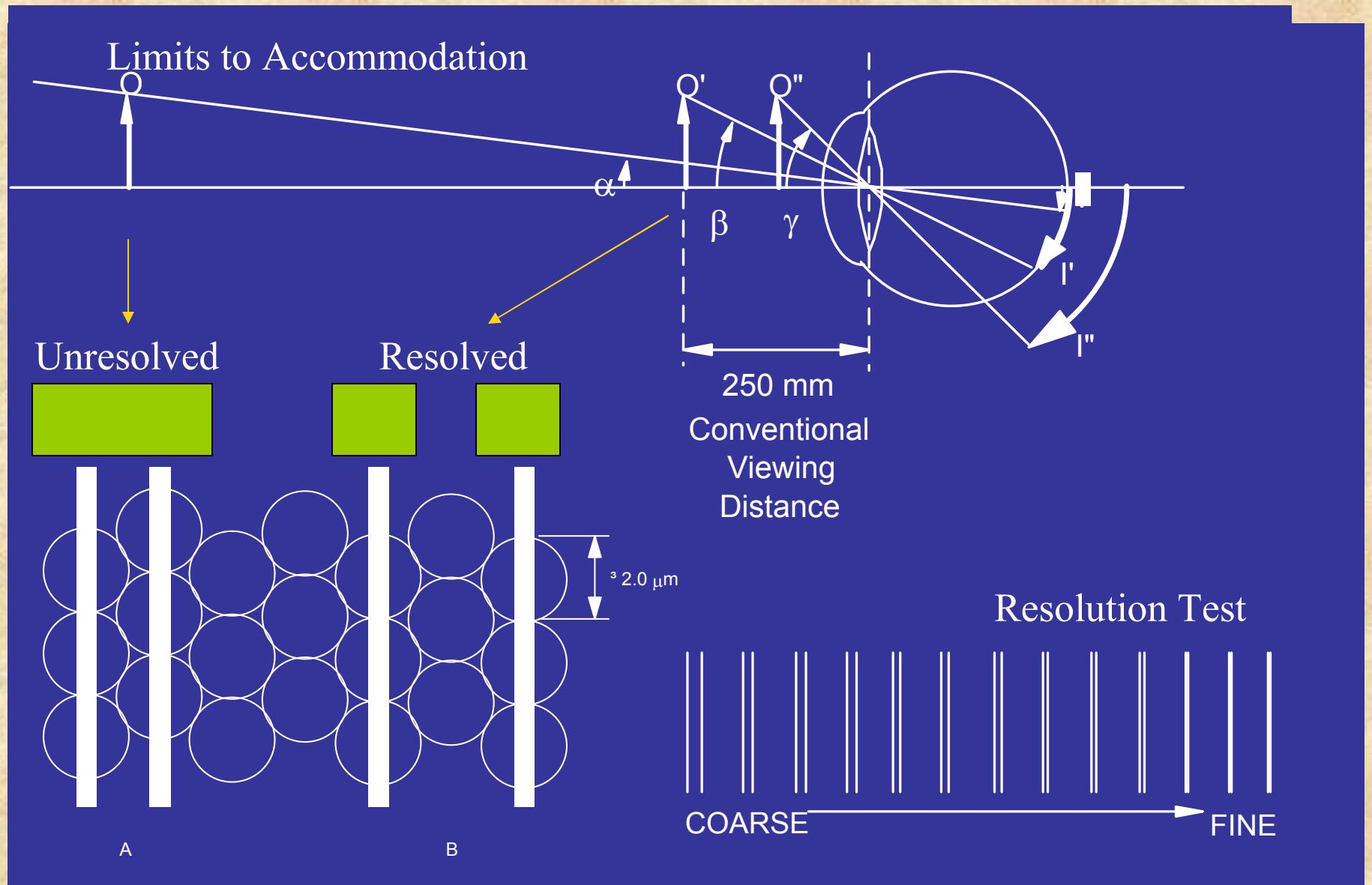
$$M_{ob} = OTL/f_{ob}$$

$$\text{Total Magnification} = M_{ob} \times M_{oc} = OTL/f_{ob} \times 250\text{mm}/f_{oc}$$

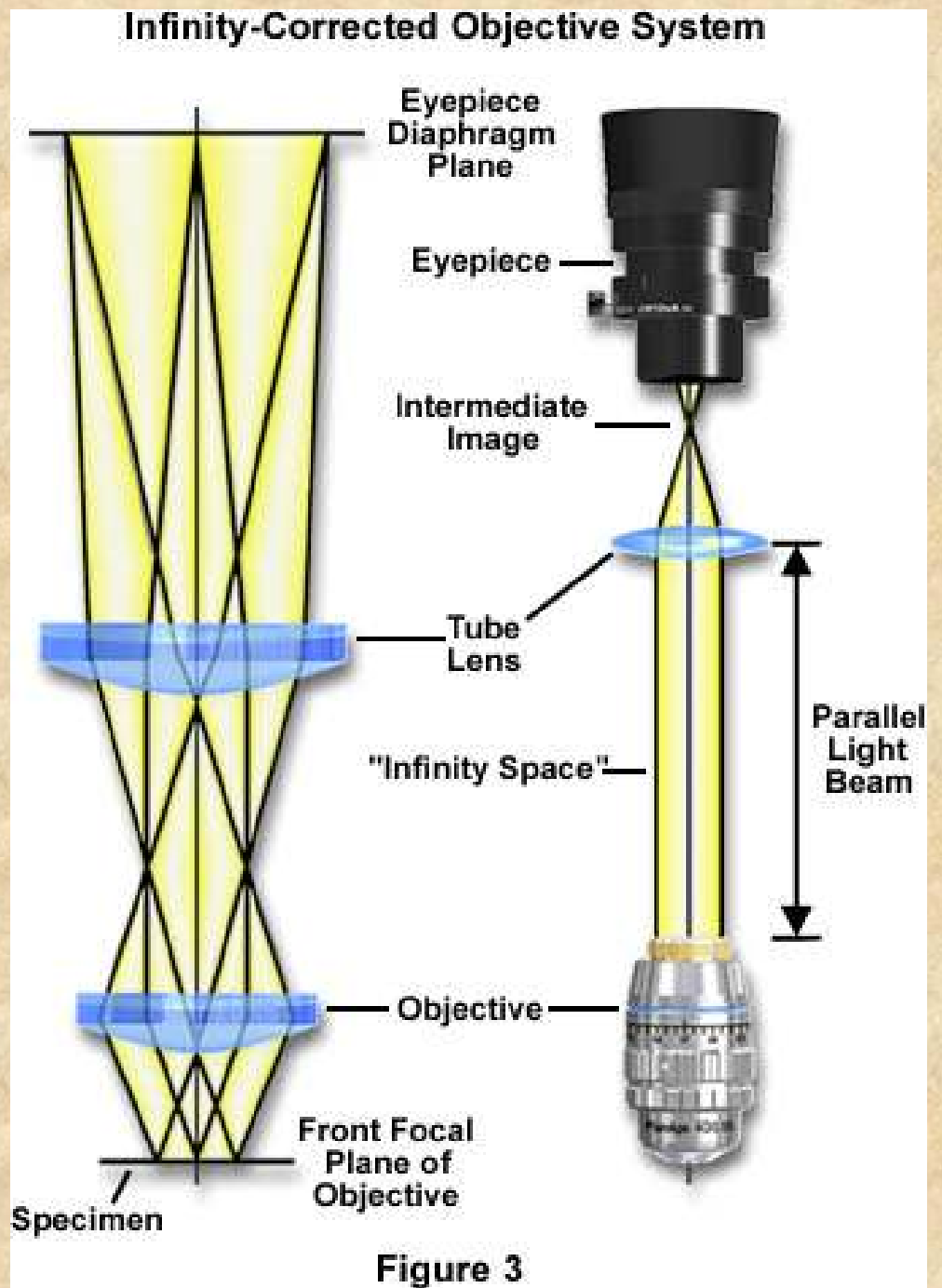
Why is the eyepiece necessary?

E.D. Salmon

Resolution Limitations of the Human Eye

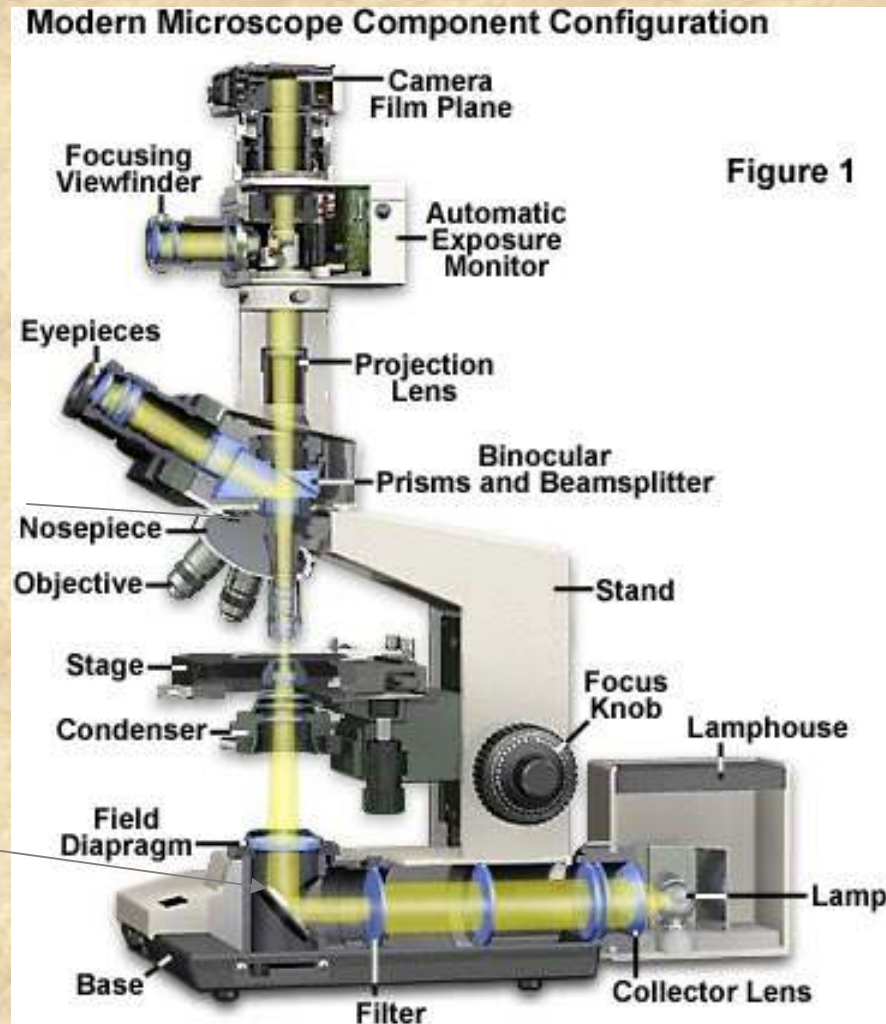


A word about infinity corrected optics and its advantages.



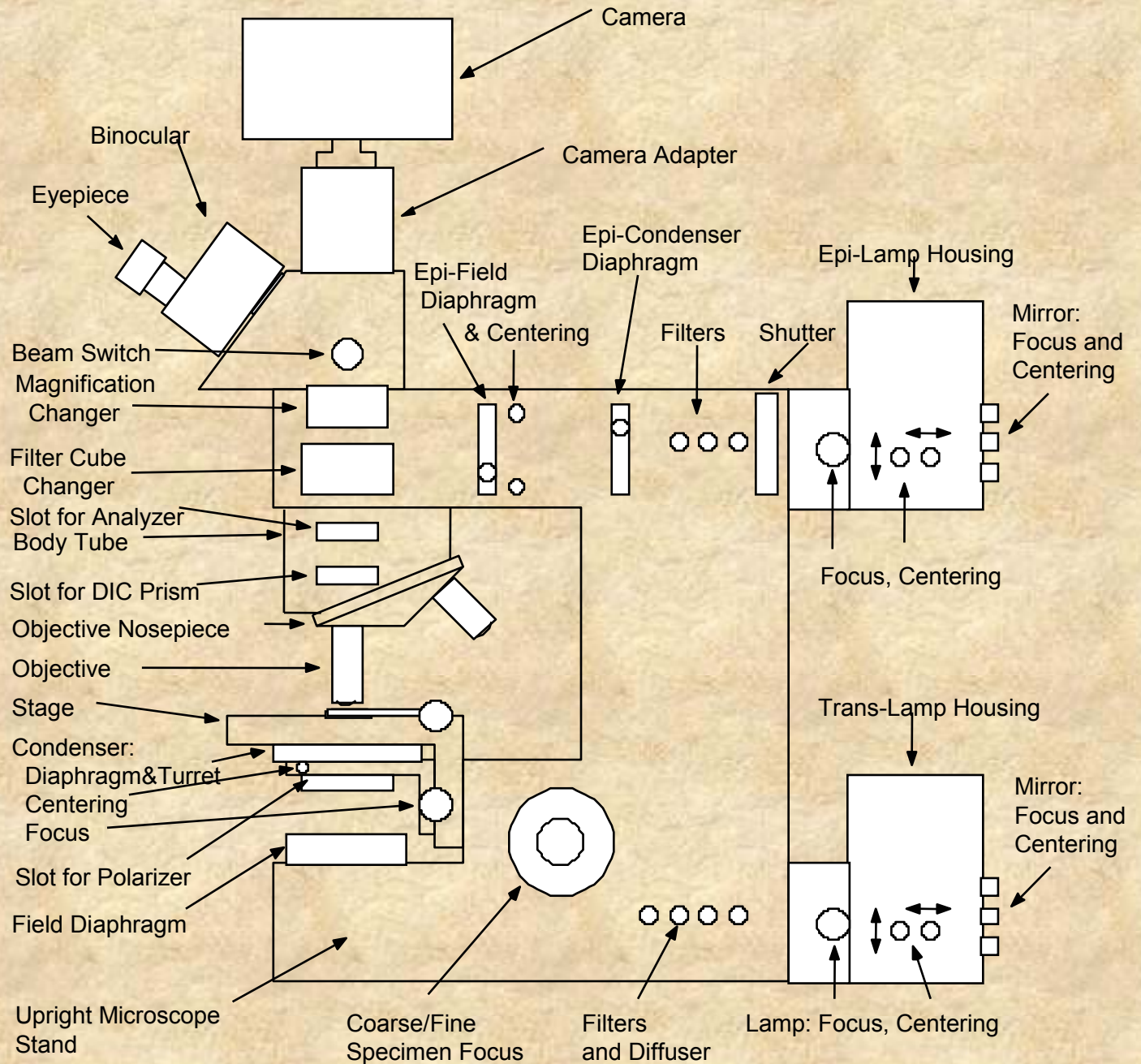
Modern microscope component identification

Prisms Used to Re-Direct Light In Imaging Path While Mirrors Are Used in Illumination Path



Identify Major Components And Their Locations And Functions Within Modern Research Light Microscope (See Salmon And Canman, 2000, Current Protocols in Cell Biology, 4.1)

MICROSCOPE COMPONENTS



Key component: the objective

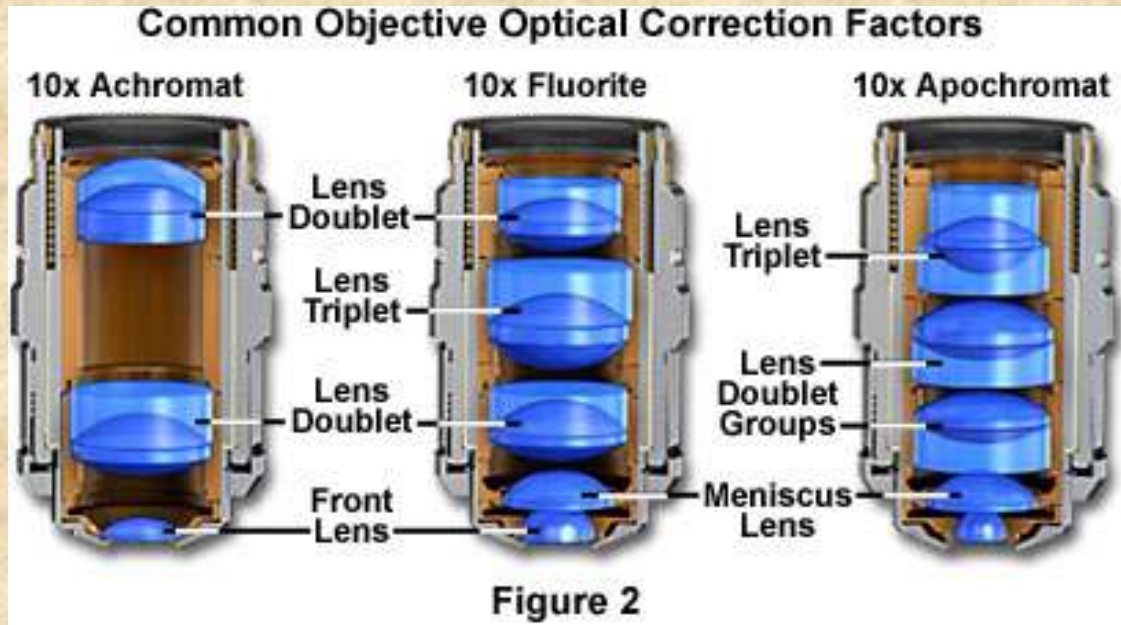
Achromats: corrected for chromatic aberration for red, blue

Fluorites: chromatically corrected for red, blue; spherically corrected for 2 colors

Apochromats: chromatically corrected for red, green & blue; spherically corrected for 2 colors

Plan-: further corrected to provide flat field

The 3 Classes of Objectives



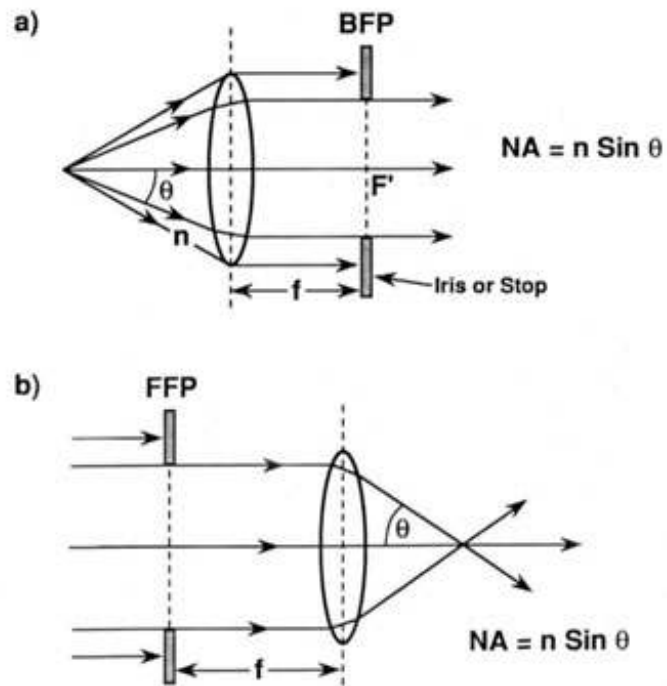
Chromatic and Mono-Chromatic Corrections



E.D. Salmon

What is numerical aperture (NA)?

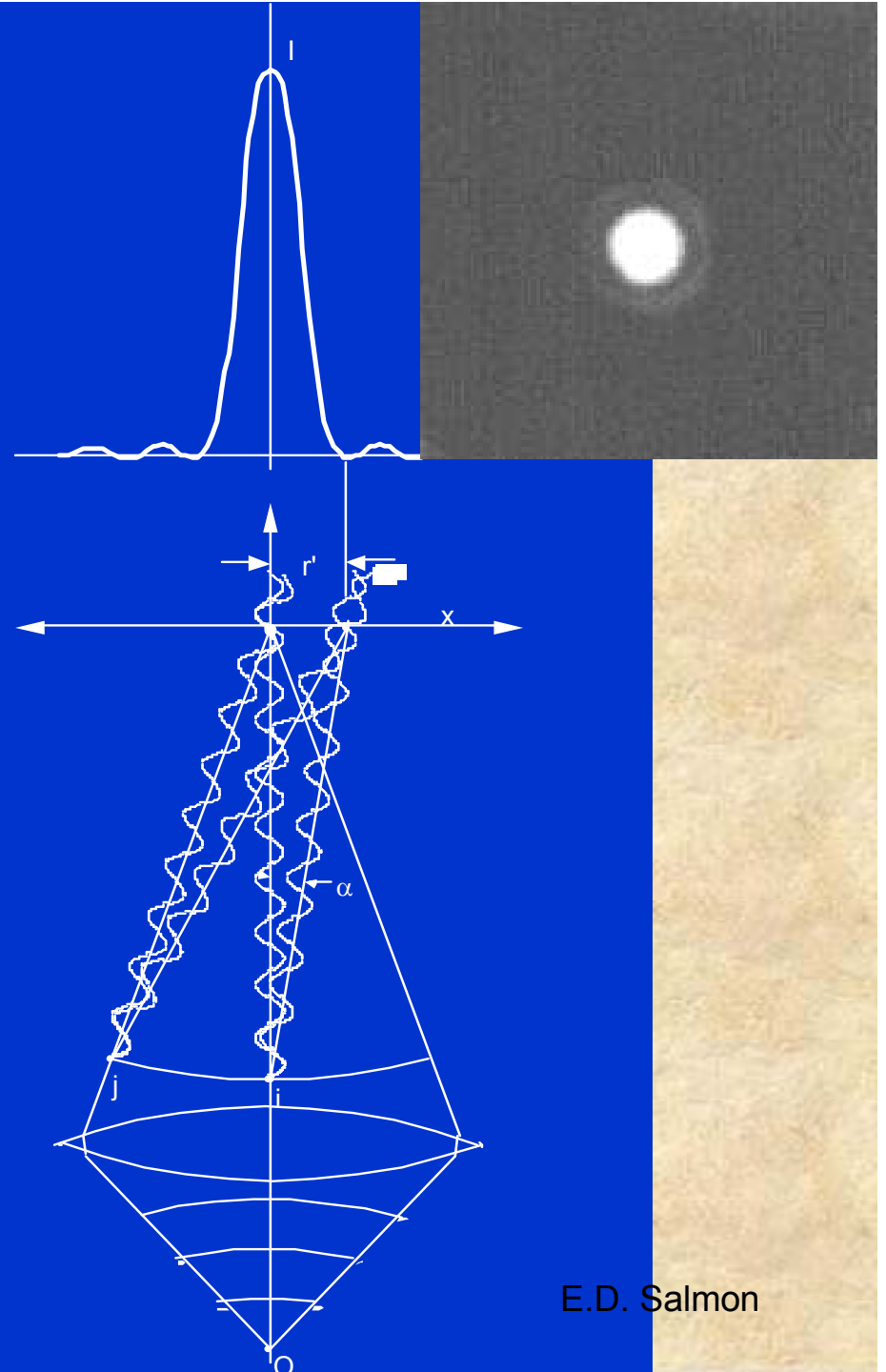
FIG. 2.1 Numerical aperture of collection (a), or illumination (b)



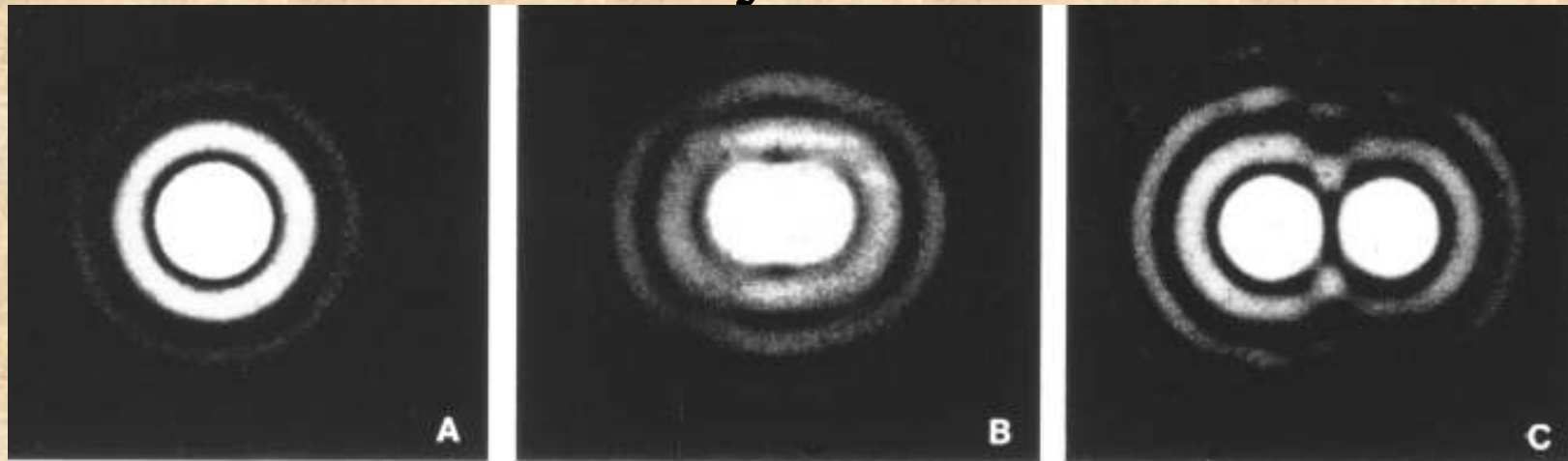
- Image Intensity: $I \sim NA_{\text{obj}}^2 / M_{\text{tot}}^2$
- Image Lateral Resolution for Corrected Objective:
 - Fluorescence: $r = 0.61\lambda / NA_{\text{obj}}$
 - Trans-Illumination: $r = \lambda / (NA_{\text{obj}} + NA_{\text{cond}})$

Airy Disk Formation by Finite Objective Aperture:

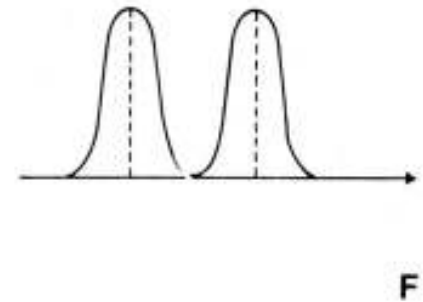
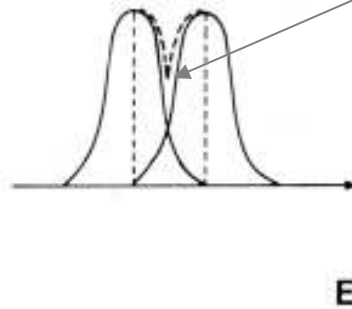
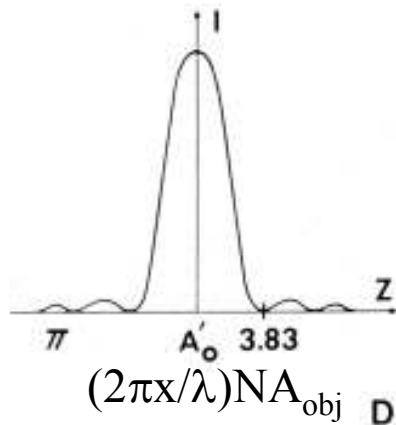
The radius of the Airy Disk at the first minimum, r' , occurs because of destructive interference; the diffraction angle, α , is given by:
 $\sin(\alpha) = 1.22\lambda/D$, where D = diameter of objective back aperture



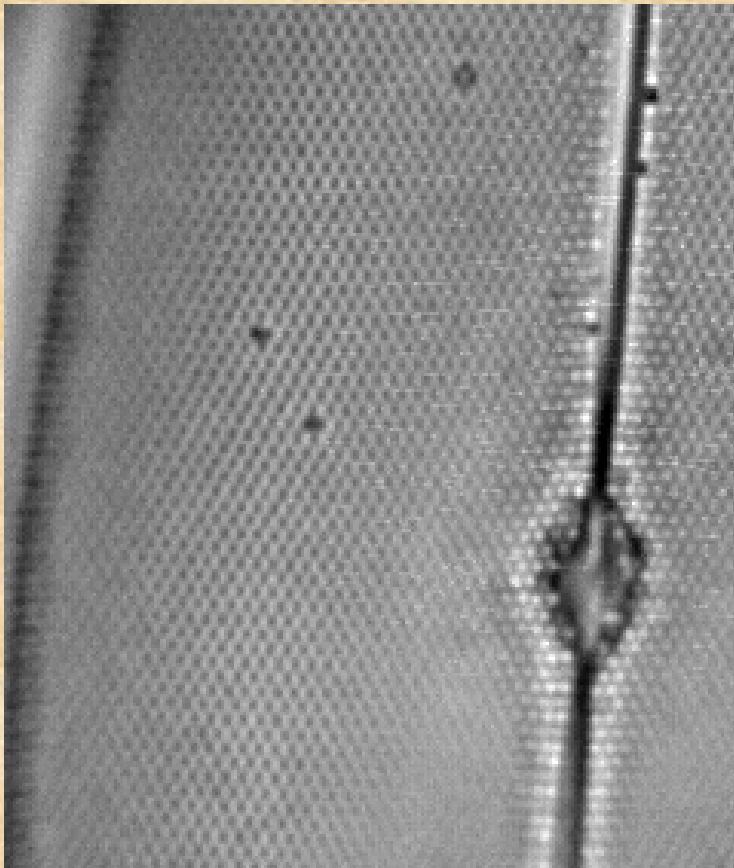
Lateral Resolution in Fluorescence Depends on Resolving Overlapping “Airy Disks”



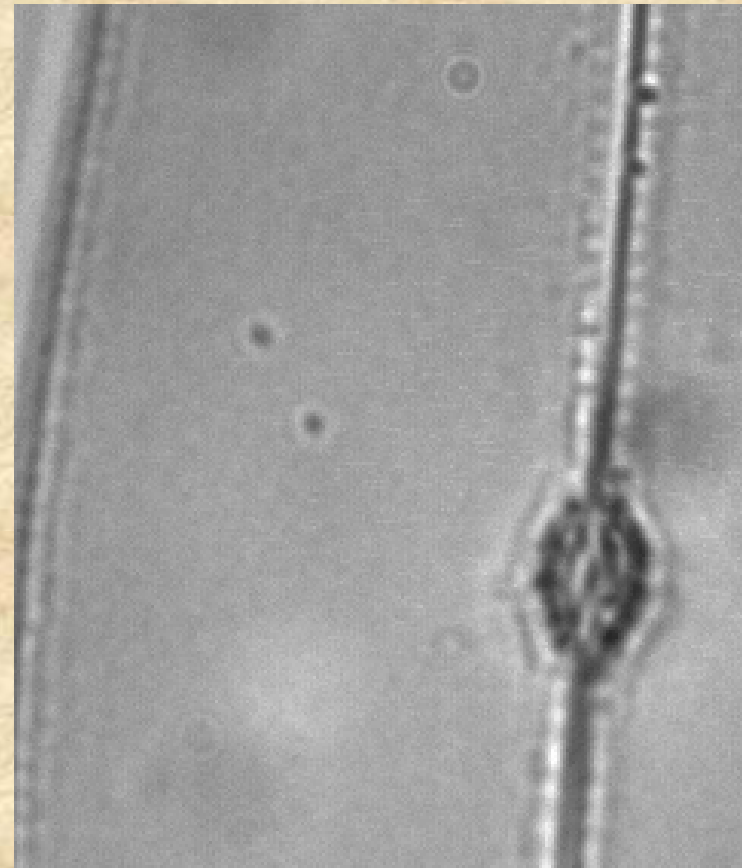
Rayleigh Criteria: Overlap by r' ,
then dip in middle is 26% below
Peak intensity



Resolution is better at shorter wavelengths,
higher objective NA or higher condenser NA



High NA and/or shorter λ



Low NA and/or longer λ

Rayleigh Criterion for the resolution of two adjacent spots:

$$P_{\text{lim}} = 0.61 \lambda_o / \text{NA}_{\text{obj}}$$

Examples: ($\lambda_o = 550 \text{ nm}$)

	Mag	f(mm)	n	a	NA	$P_{\text{lim}} (\mu\text{m})$	($\text{NA}_{\text{cond}} = \text{NA}_{\text{obj}}$)
high dry	10x	16	1.00	15	0.25	1.10	
	40x	4	1.00	40	0.65	0.42	
oil	100x	1.6	1.52	61	1.33	0.204	
	63x	2.5	1.52	67.5	1.40	0.196	

Why oil immersion lenses have greater resolution

Oil Immersion and Numerical Aperture

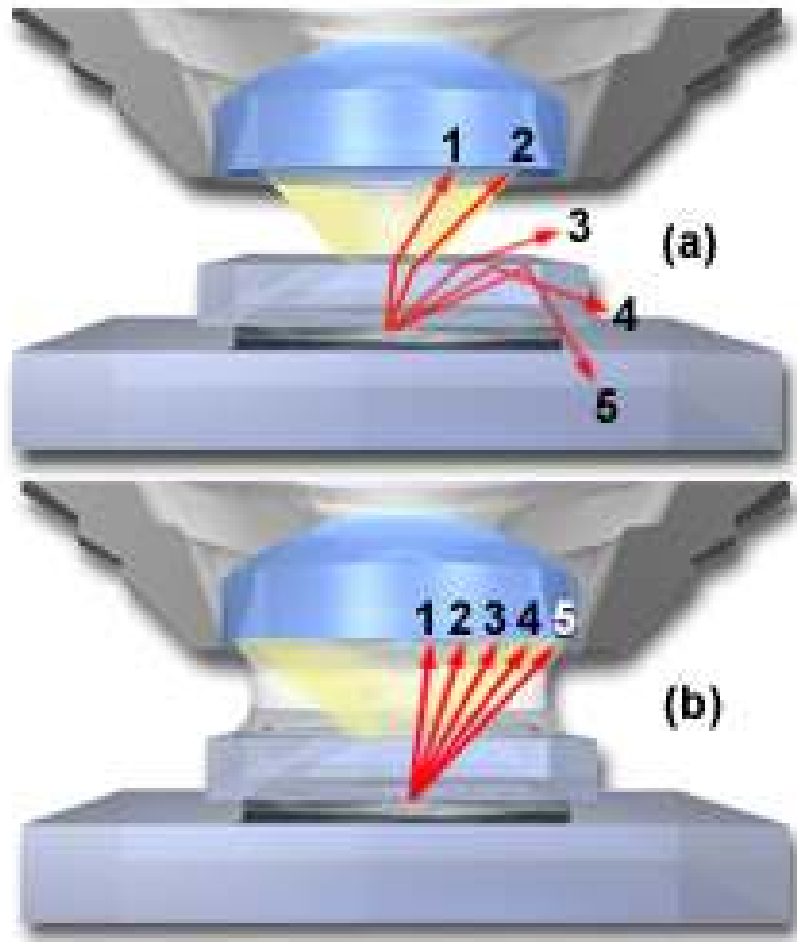


Figure 1

$$D = 0.61 \lambda \cos \alpha / n(\text{NA})^2$$

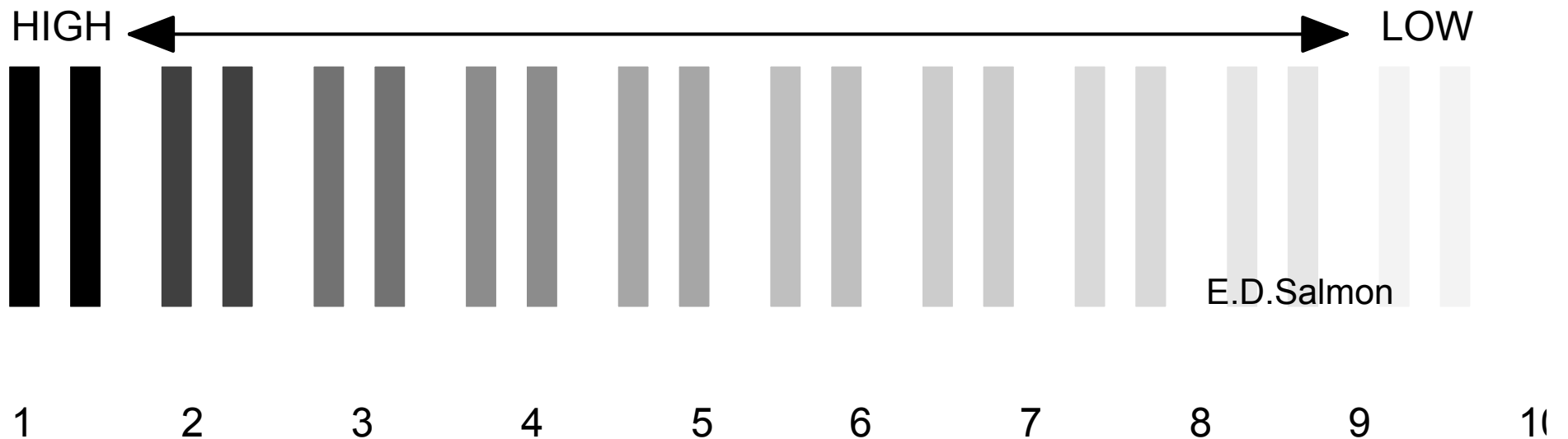
Low power, NA~ 0.25 D~ 8 μm

Hi, dry, NA~0.5 D~ 2 μm

Oil immersion, NA~ 1.3 D~0.4 μm

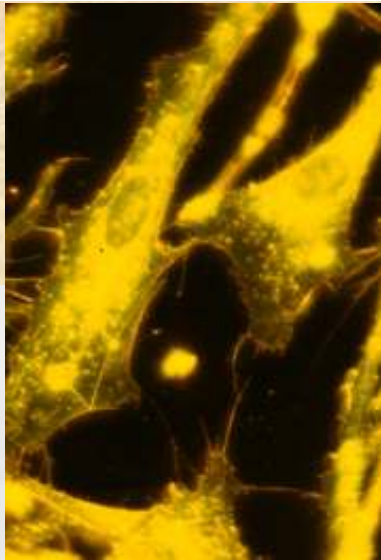
Contrast : All the resolution in the world won't do you any good, if there is no contrast to visualize the specimen.

$$\text{CONTRAST} = (I_{sp} - I_{bg}) / I_{bg}$$

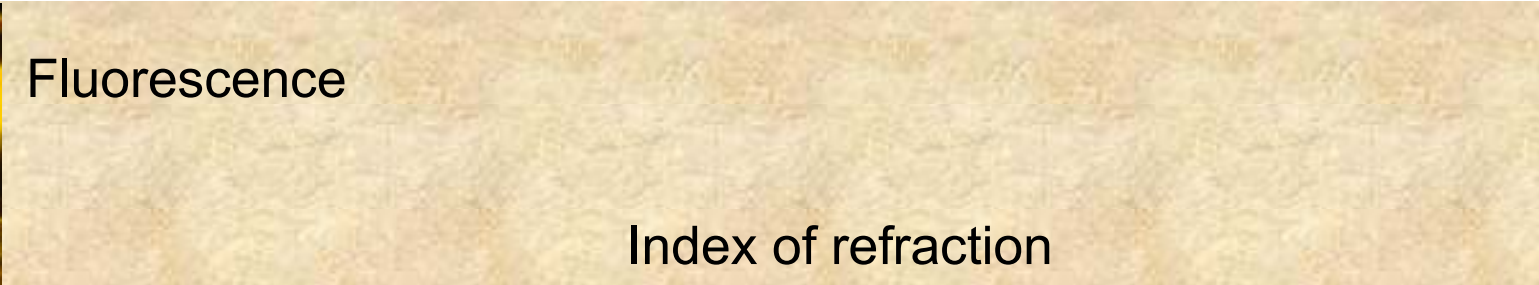


CONTRAST MODES OF LIGHT MICROSCOPY

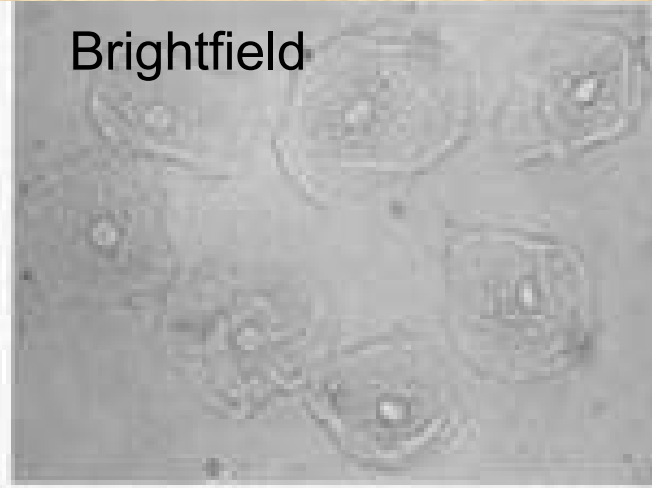
MODE	MECHANISM OF CONTRAST
Brightfield	Absorption of light
Phase contrast	Optical path length (index, density)
DIC	Rate of change of optical path
Widefield fluorescence	Absorption of light, quantum yield of fluorophore
Confocal fluorescence	same as fluorescence
Darkfield	light scattering by edges in specimen
Interference reflection contrast	interference between reflections from ventral cell surface and substratum
Polarization	Extinction between crossed polars caused by specimen birefringence



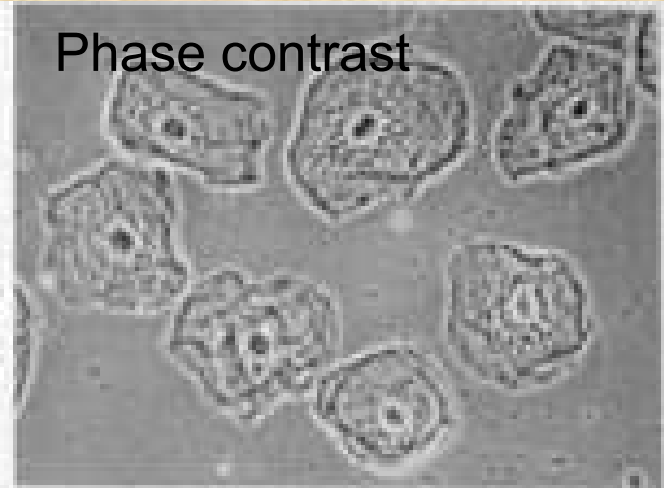
Fluorescence



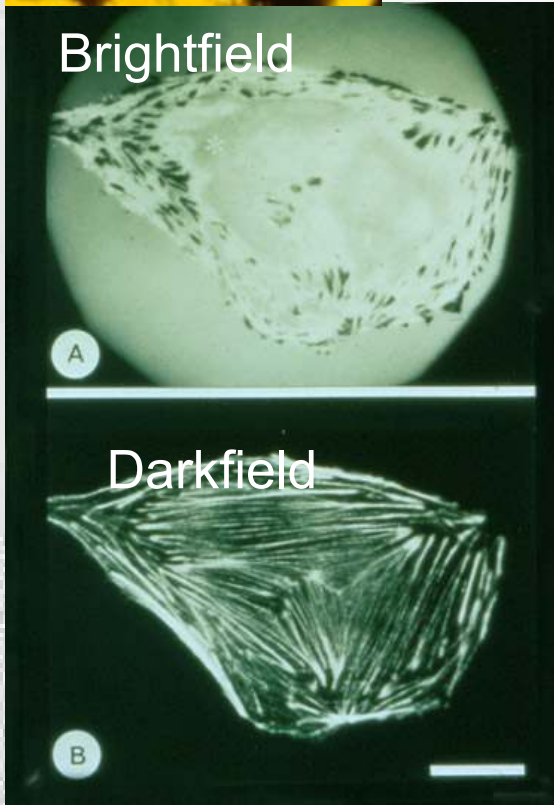
Index of refraction



Brightfield



Phase contrast



Brightfield

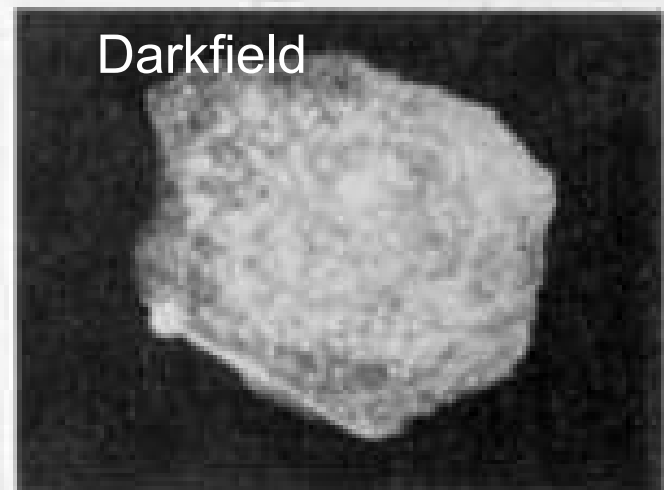
A

Darkfield

B

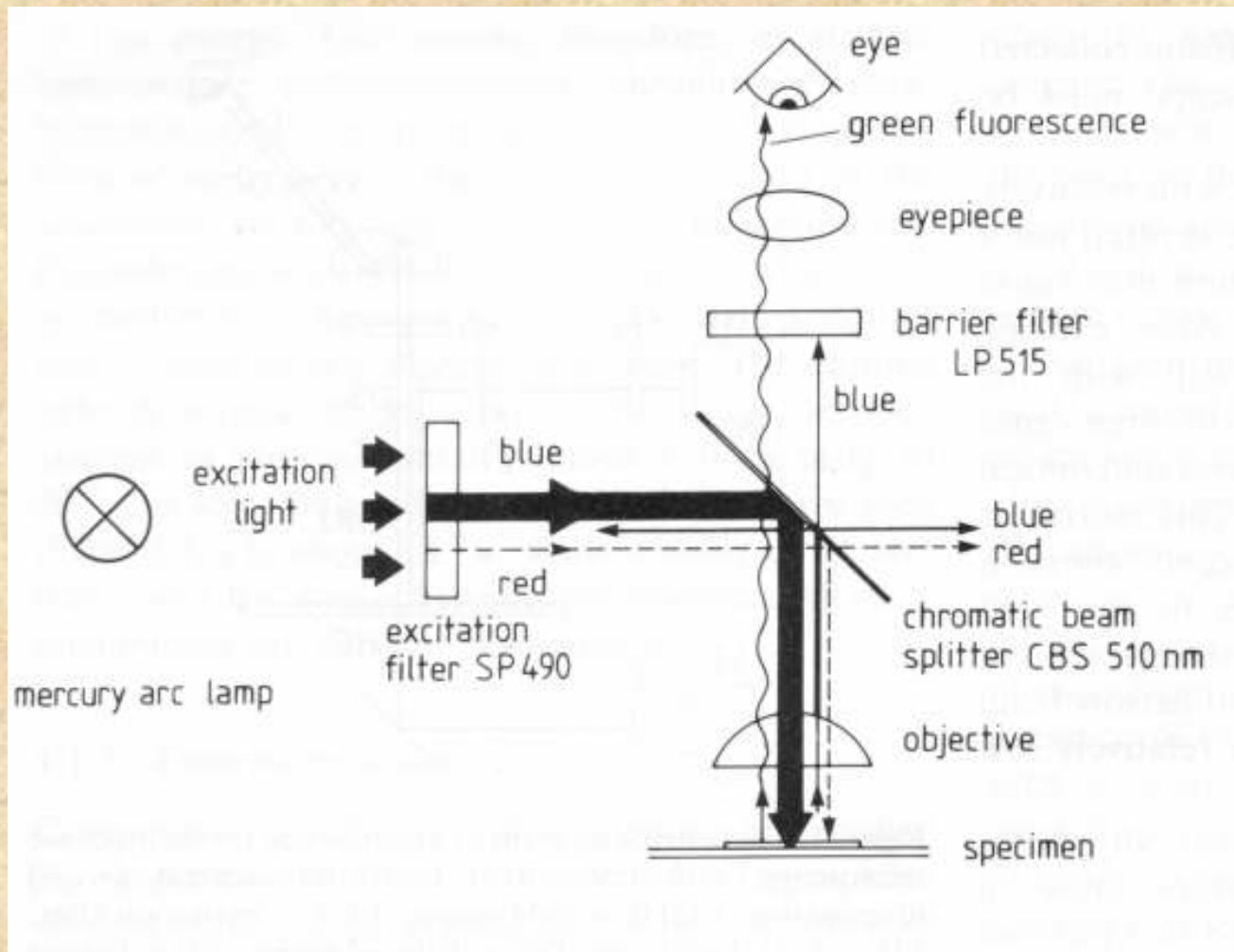


Normalized interference



Darkfield

Basic design of the epi fluorescence microscope



Objectives

High transmittance

Fluorite lenses: $\lambda > 350$ nm [ok for FURA]

Quartz lenses: $\lambda < 350$ nm

Employ simple, non plan lenses to minimize internal elements.

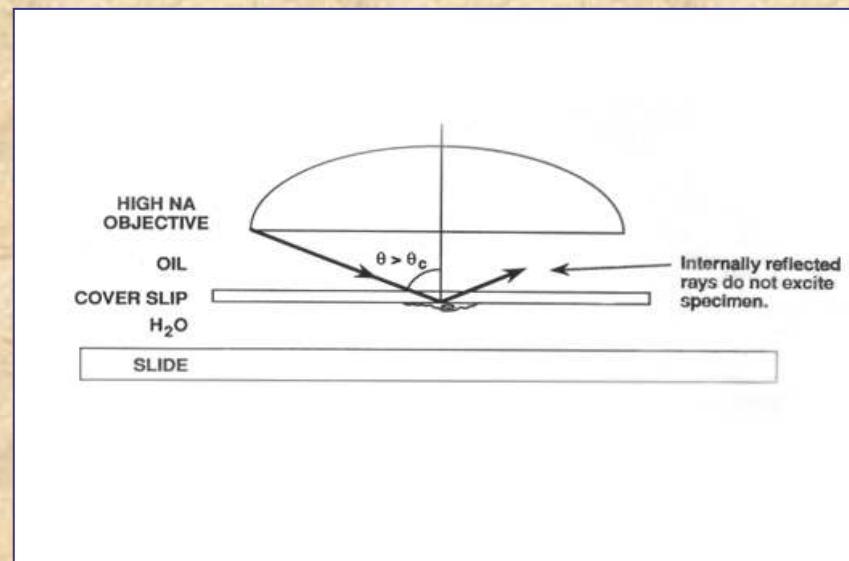
Negligible auto-fluorescence or solarization [color change upon prolonged illumination]

Maximizing image brightness (B)

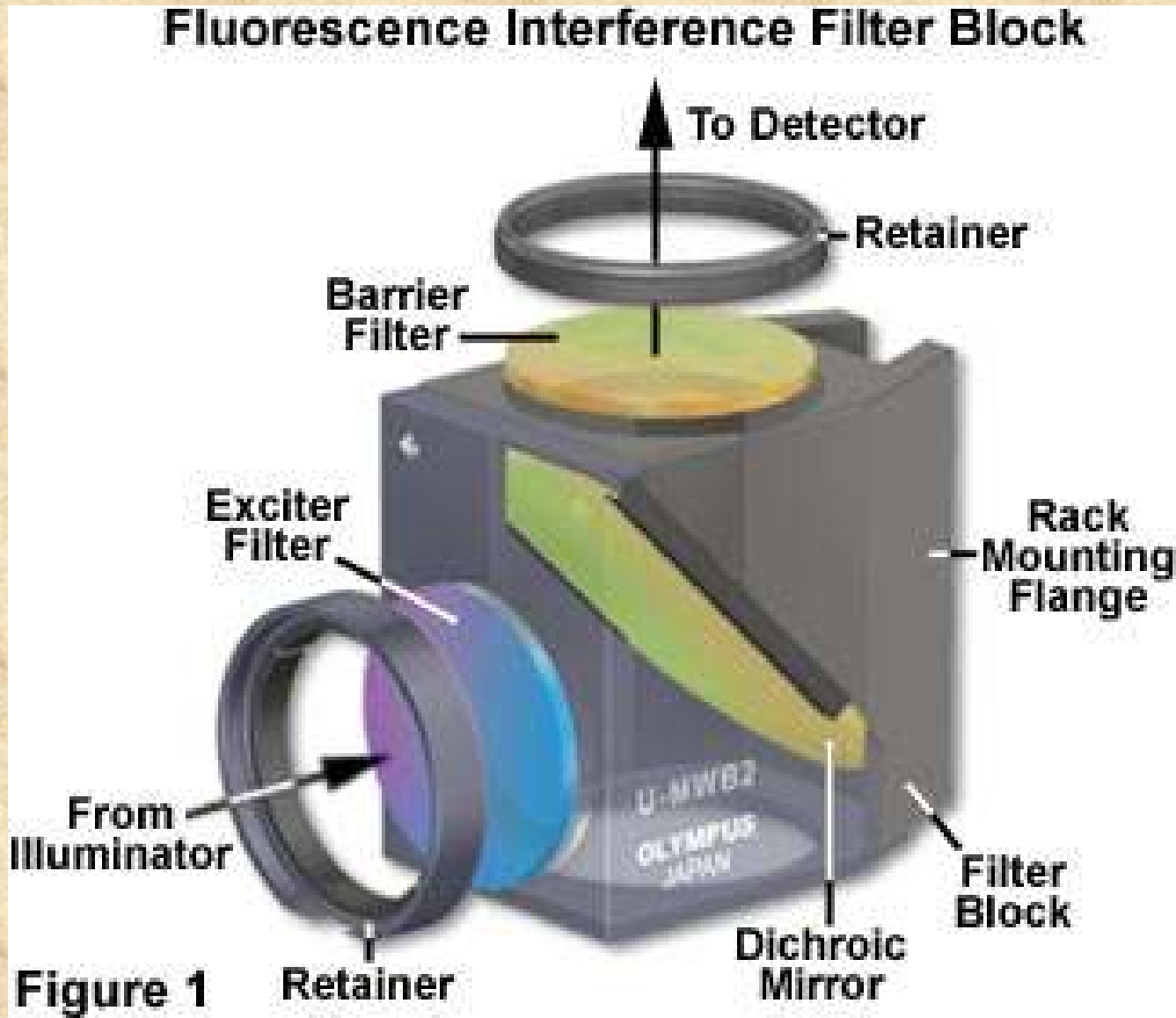
$$\left. \begin{array}{l} \text{excitation efficiency} \sim (NA)^2 \\ \text{collection efficiency} \sim (NA)^2 \end{array} \right\} \Rightarrow B \sim (NA)^4$$

$$\text{also } B \sim \frac{1}{M^2} \Rightarrow B \sim \frac{(NA)^4}{M^2}, \text{ for } NA \leq 1.0$$

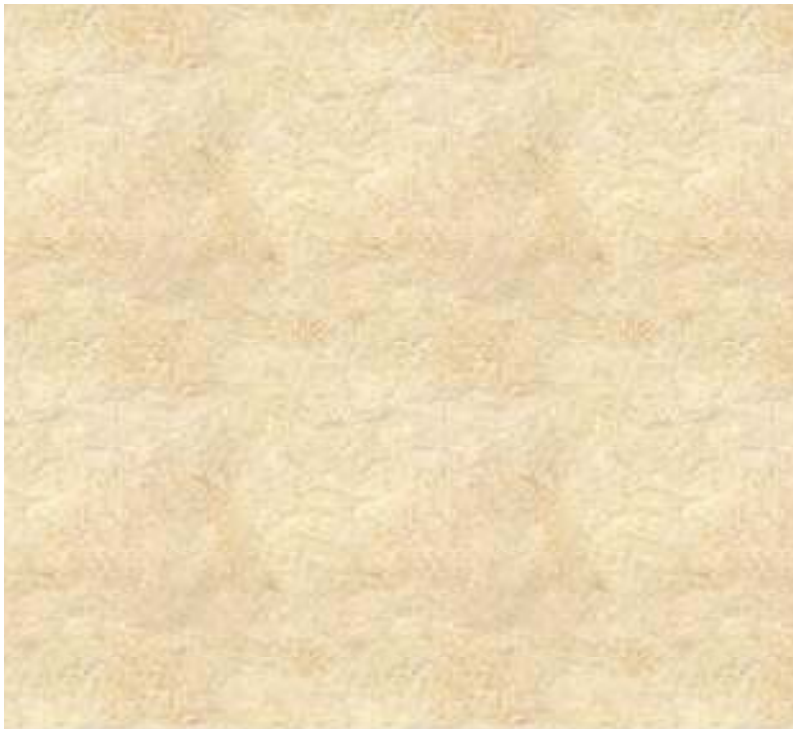
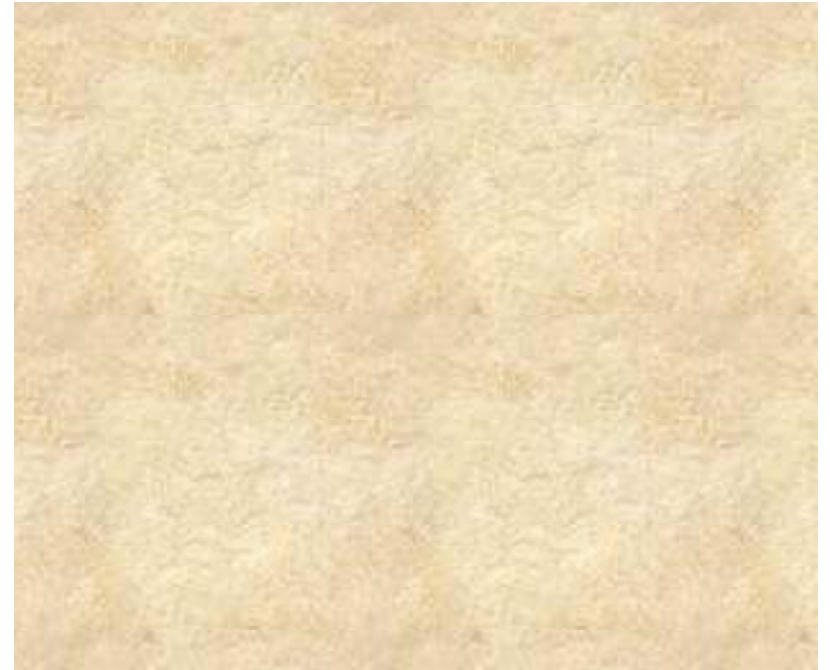
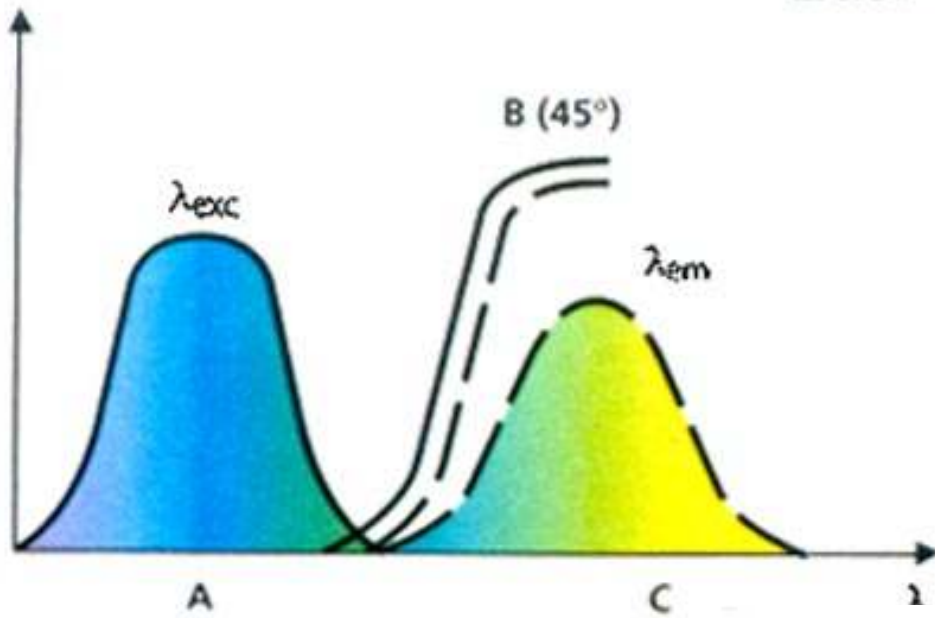
at high NA,



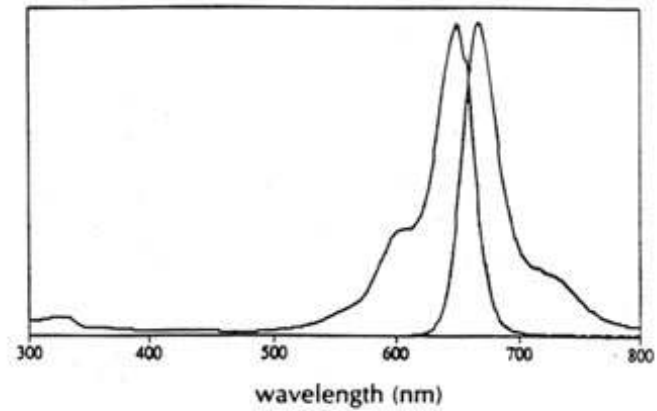
Filters



Zeiss

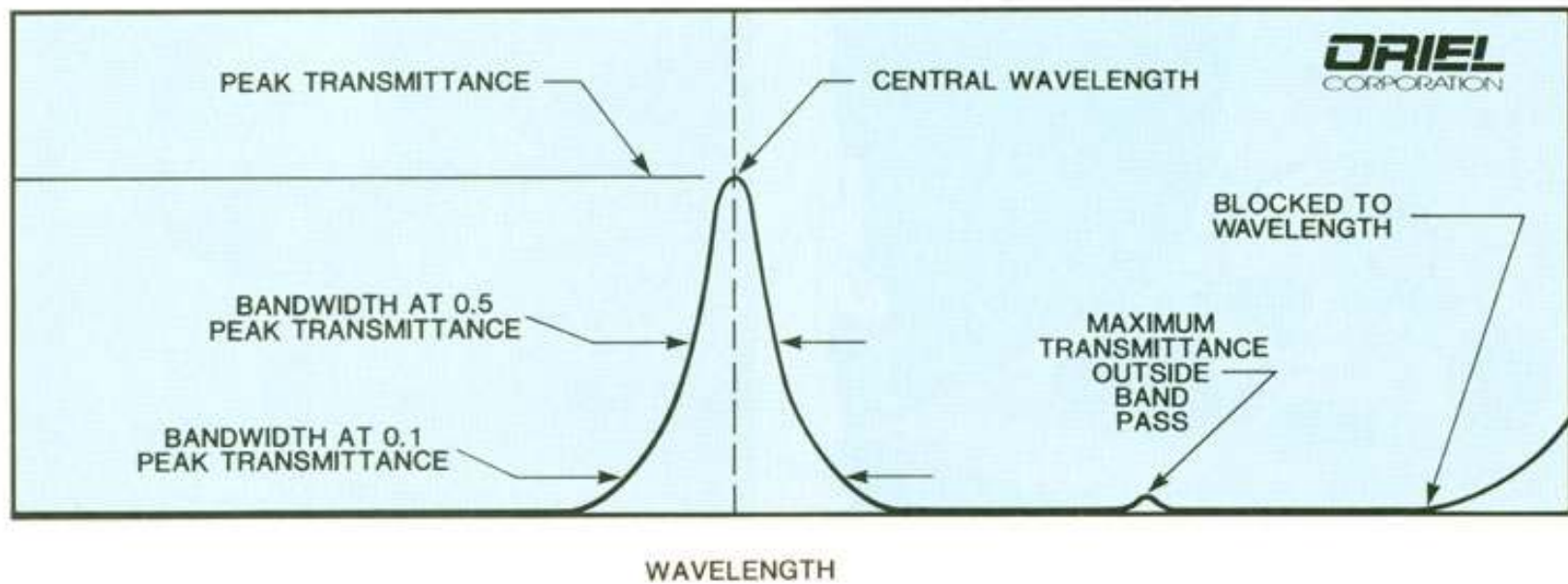


Cy5-methylamine conjugate



Abs. max.	652 nm
Ext. max.	$> 200,000 \text{ M}^{-1}\text{cm}^{-1}$
Fluor. max.	667 nm
Q. Y. (Ab,N~2)	0.28

Interference filter definitions



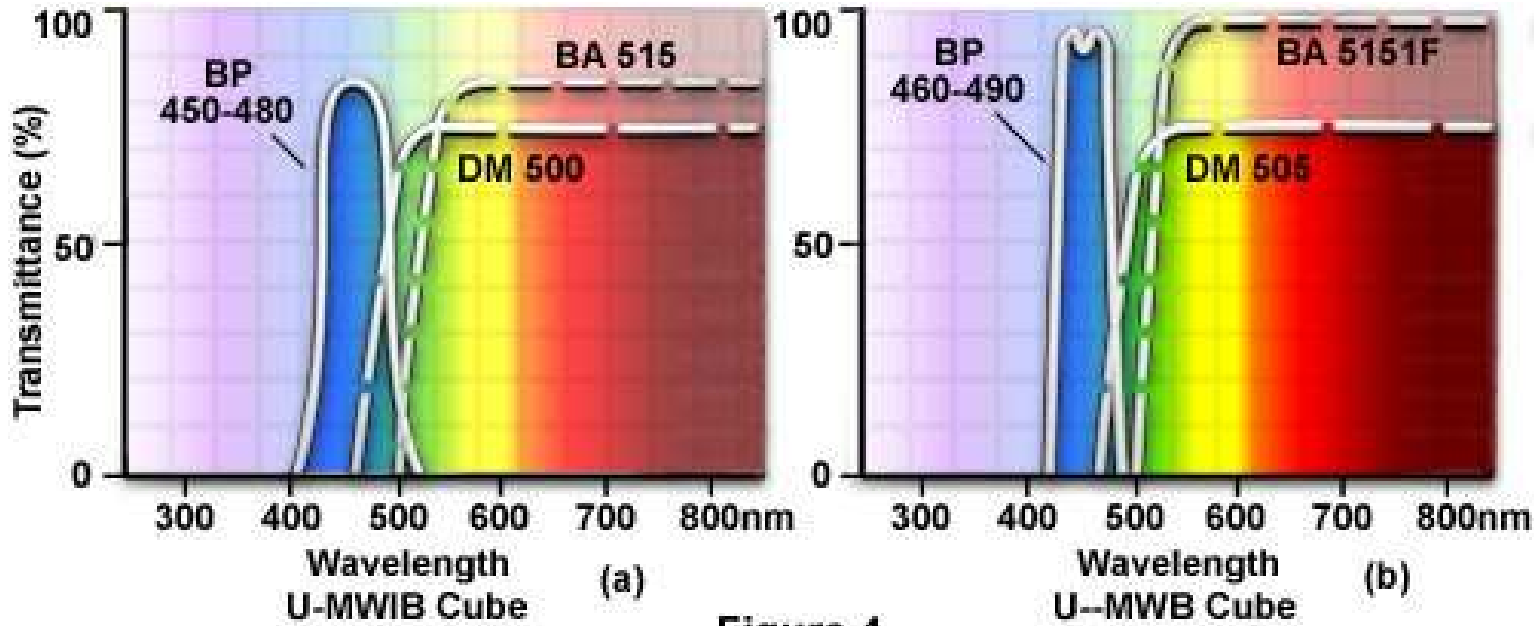


Figure 4

Filter cube designs employing long-pass emitter filters

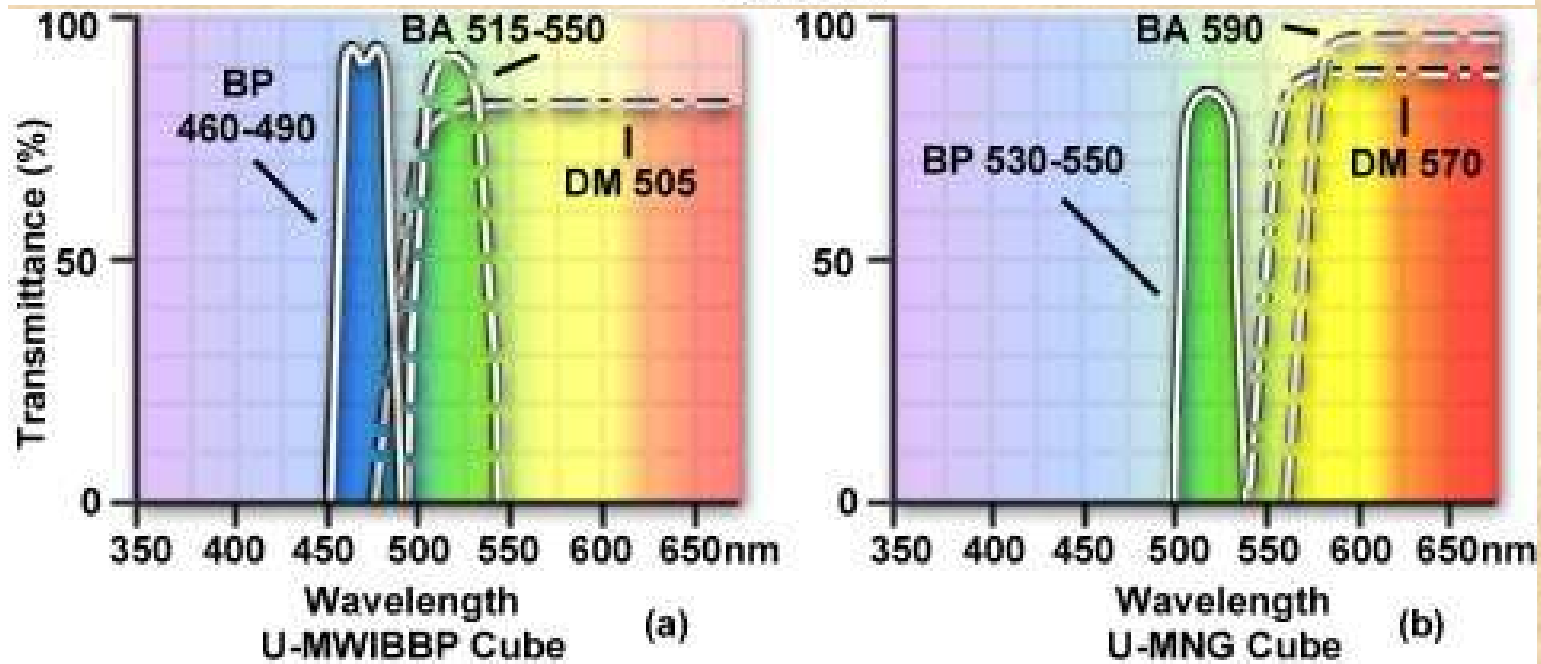


Figure 5

Filter cube designs employing band-pass emitter filters

Multi-Wavelength Immunofluorescence Microscopy

Bovine Pulmonary Artery Epithelial Cells

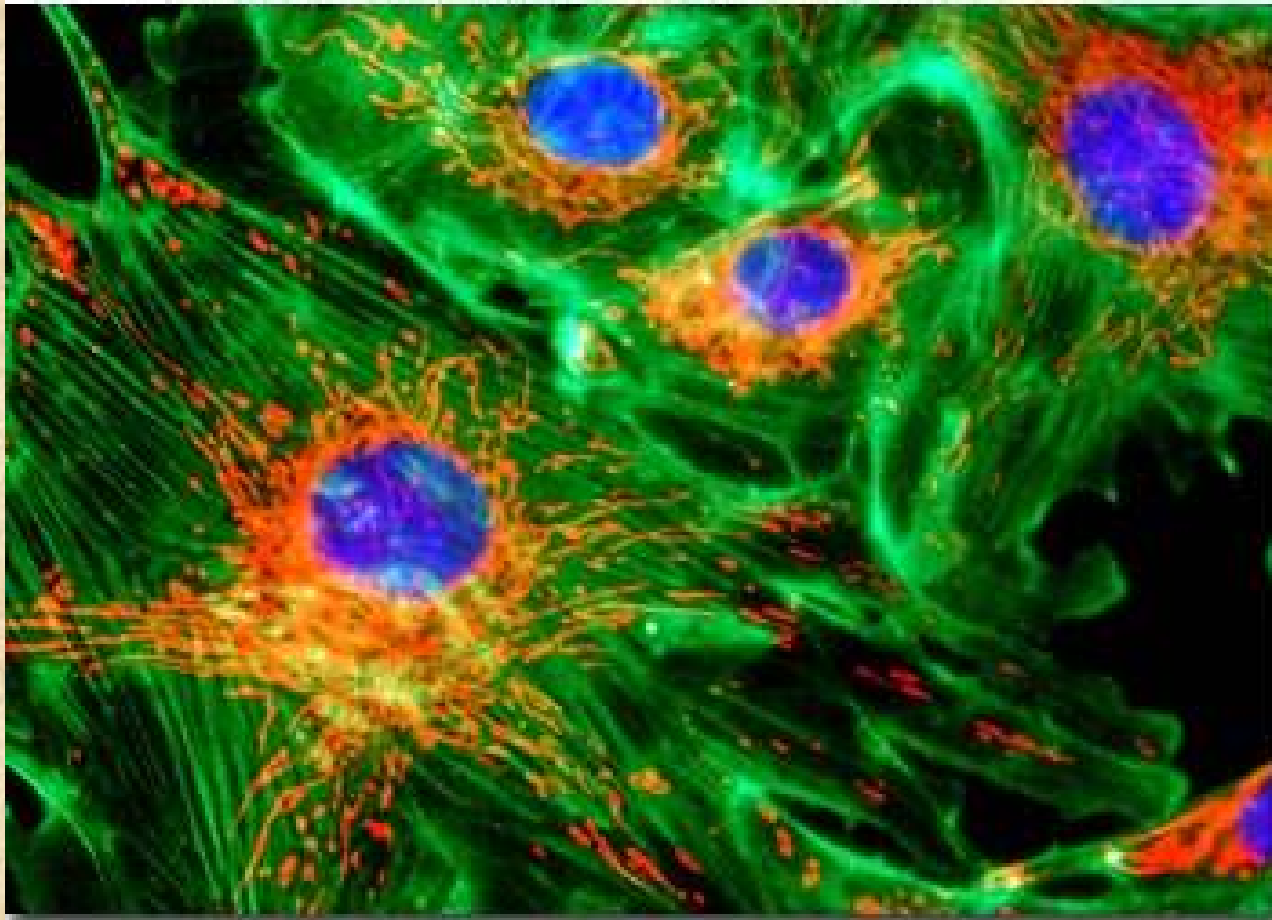
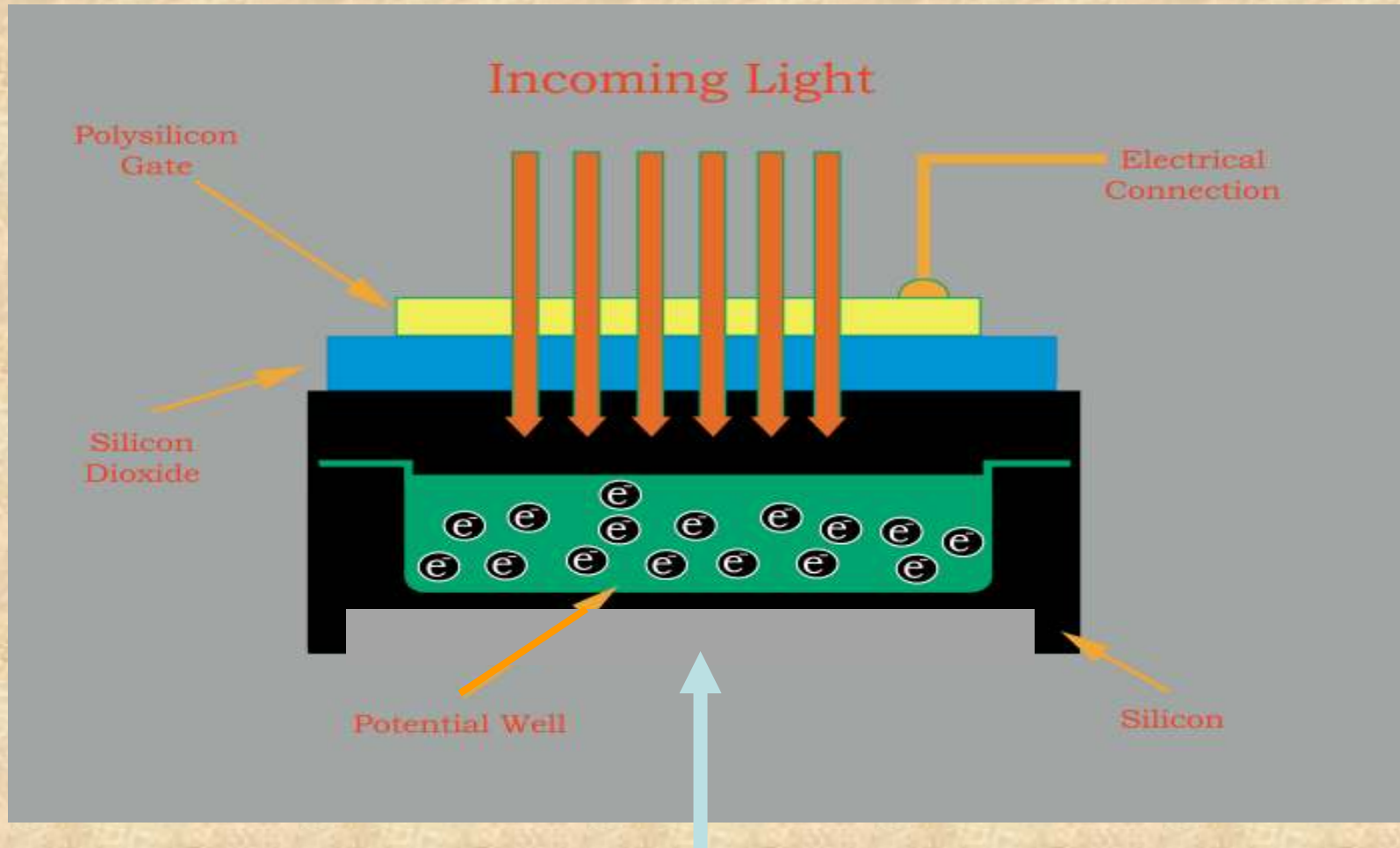


Figure 1

PIXELS

The building blocks of CCDs



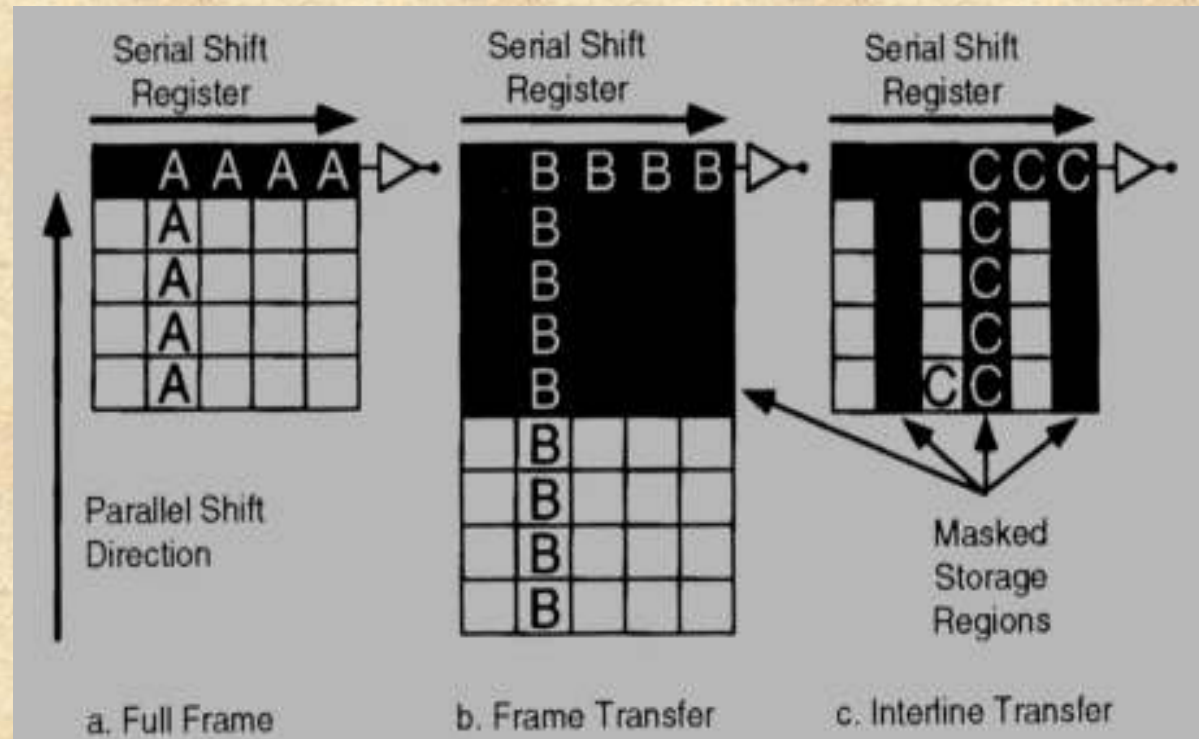
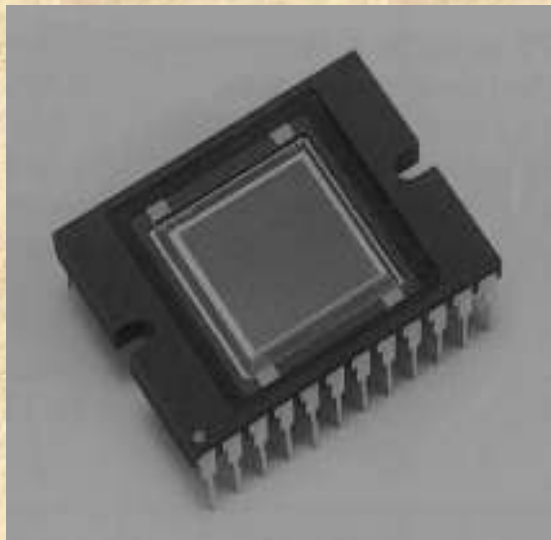
Back thinned CCDs receive light from this side

Primary Features of CCD

- **Spatial resolution of the CCD array**
 - Number of Pixels in X and Y
 - Center to Center Distance of Pixels in microns
- **Full Well Capacity**
 - Related to Physical size and electronic design
 - Determines Maximum Signal level possible
- **Quantum Efficiency/Spectral Range**
 - Determines the usefulness of the camera
 - Major influence on exposure time
- **Camera Noise**
 - The limiting feature in low light applications
 - Influenced by Readout Speed / Readout Noise
 - Influenced by Dark Current / Time
- **CCD Chip Design**
 - Influences Total Frame Rate
 - Exposure time plus Readout time
 - Total Photon Efficiency
 - Quantum Efficiency and Exposure Cycle

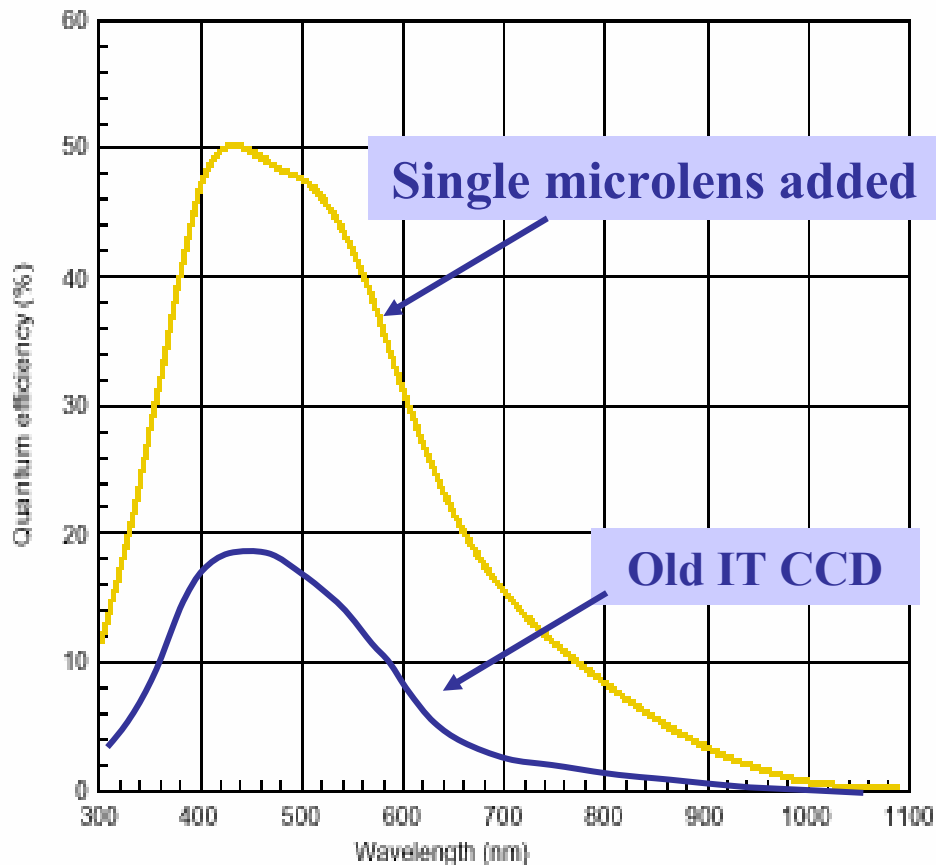
Types of CCD Detectors

- CCD Cameras - 3 Primary Designs

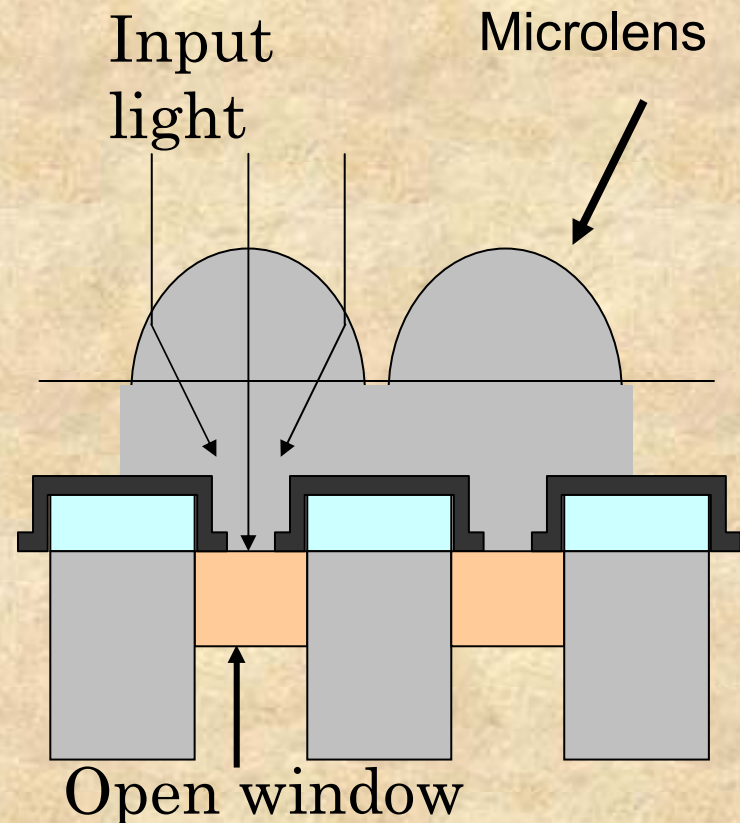


Improvements in Interline CCDs

- Effective Q.E. was greatly increased by Microlens technology.



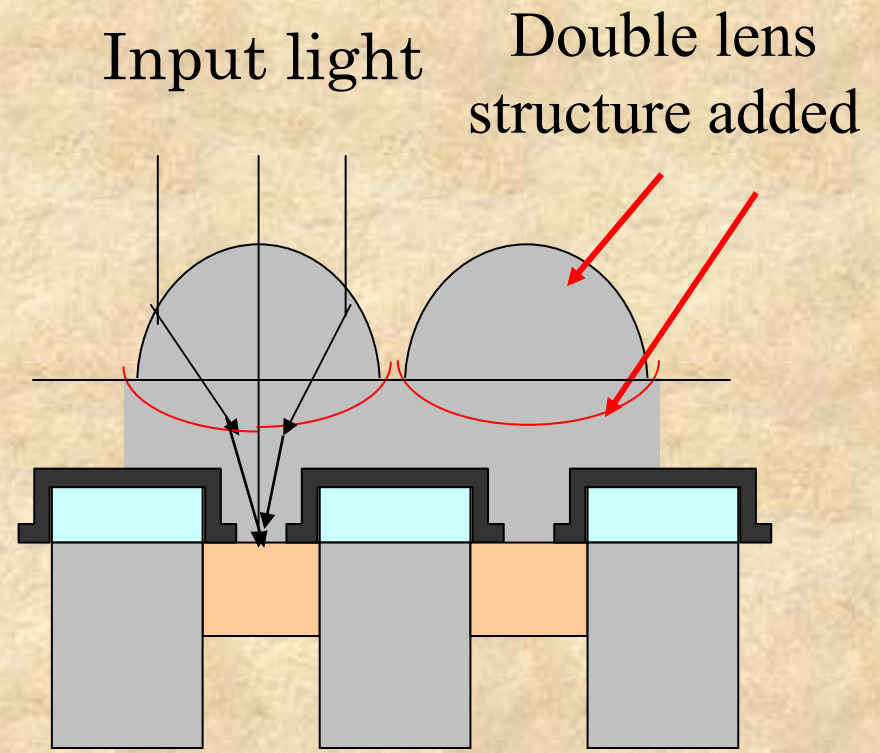
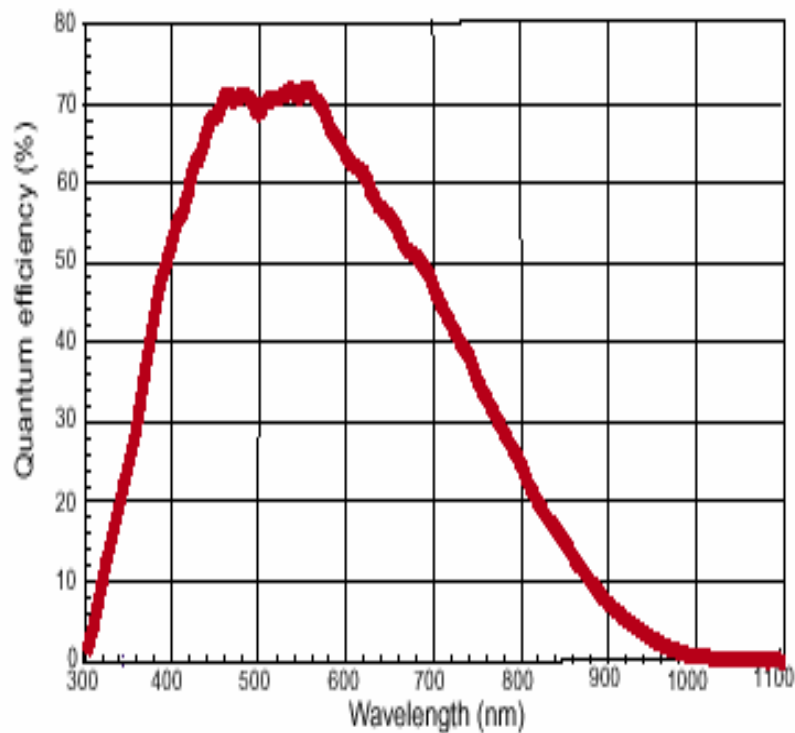
B. Moomaw, Hamamatsu Corp.



Latest Improvement to Interline CCDs

- Latest double micro lens structure improved the CCD open ratio up to 80% and Q.E. to over 70%!

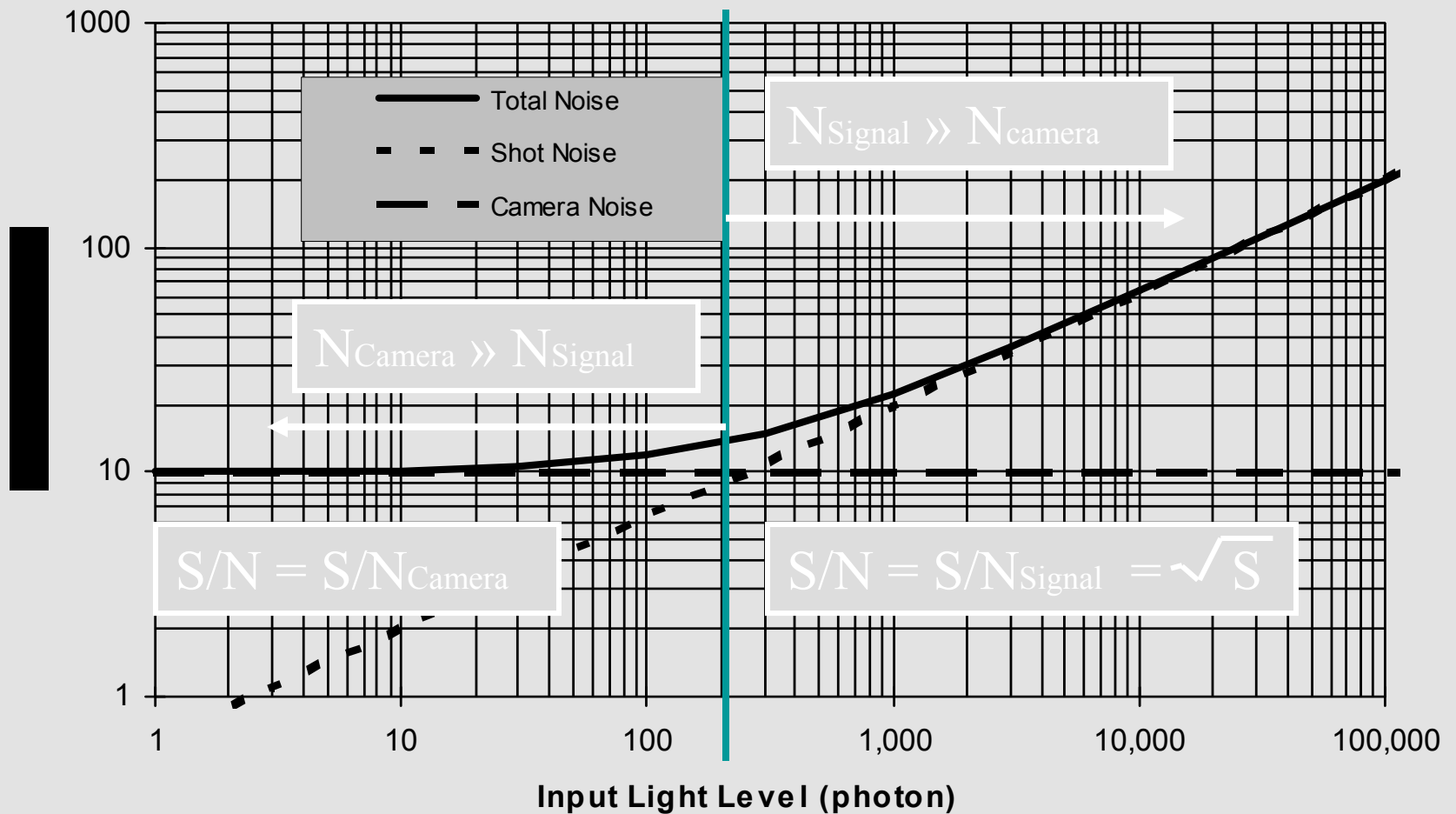
SPECTRAL RESPONSE CHARACTERISTICS



B. Moomaw, Hamamatsu Corp.

Noise as a function of incident camera illumination

(Camera Noise = 10 electron, QE = 0.4)



COMMON SOURCES OF AUTOFLUORESCENCE

<u>Autofluorescent Source</u>	<u>Typical Emission Wavelength (nm)</u>	<u>Typical Excitation Wavelength (nm)</u>
Flavins	520 to 560	380 to 490
NADH and NADPH	440 to 470	360 to 390
Lipofuscins	430 to 670	360 to 490
Advanced glycation end-products (AGEs)	385 to 450	320 to 370
Elastin and collagen	470 to 520	440 to 480
Lignin	530	488
Chlorophyll	685 (740)	488

From Biophotonics International

Photobleaching

- *Photochemical lifetime*: fluorescein will undergo 30-40,000 emissions before bleaching. ($QY_{\text{bleaching}} \sim 3 \times 10^{-5}$)
- At low excitation intensities, photobleaching occurs but at lower rate.
- Bleaching is often photodynamic--involves light and oxygen.

Parameters for Maximizing Sensitivity

- Use High Objective NA and Lowest Magnification:

$$I_{fl} \sim I_{il} NA_{obj}^4 / M_{tot}^2$$

-Buy the newest objective: select for best efficiency

- Close Field Diaphragm down as far as possible
- Use high efficiency filters
- Use as few optical components as possible
- Match magnification to camera resolution:

$$M_{Max} = 3 * \text{Pixel Size of Detector} / \text{Optical Resolution}$$

$$\text{E.g.: } 3 * 7 \mu\text{m} / [0.6 * 520\text{nm} / 1.4] = 91X$$

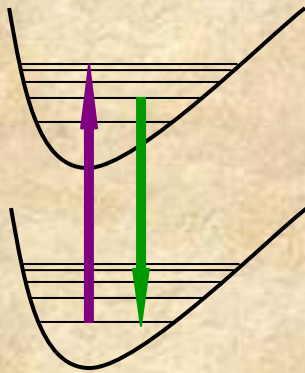
- Reduce Photobleaching
- Use High Quantum Efficiency Detector in Camera

Live Cell Considerations

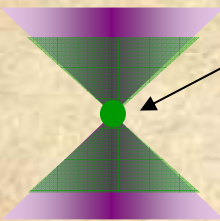
- Minimize photobleaching and photodamage (shutters)
- Use heat reflection filters for live cell imaging
- Image quality: Maximize sensitivity and signal to noise (high transmission efficiency optics and high quantum efficiency detector)
- Phase Contrast is Convenient to Use with Epi-Fluorescence
 - Use shutters to switch between fluorescence and phase
 - Phase ring absorbs $\sim 15\%$ of emission and slightly reduces resolution by enlarging the PSF

Defining Our Observation Volume: One- & Two-Photon Excitation.

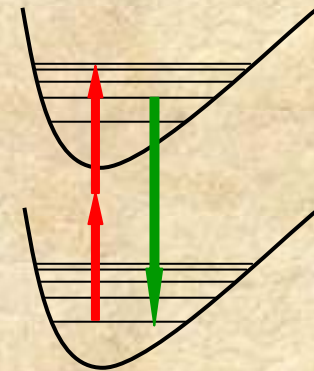
1 - Photon



Defined by the pinhole size,
wavelength, magnification
and numerical aperture of
the objective

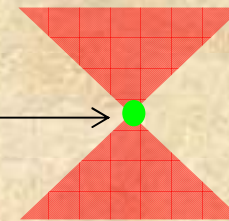


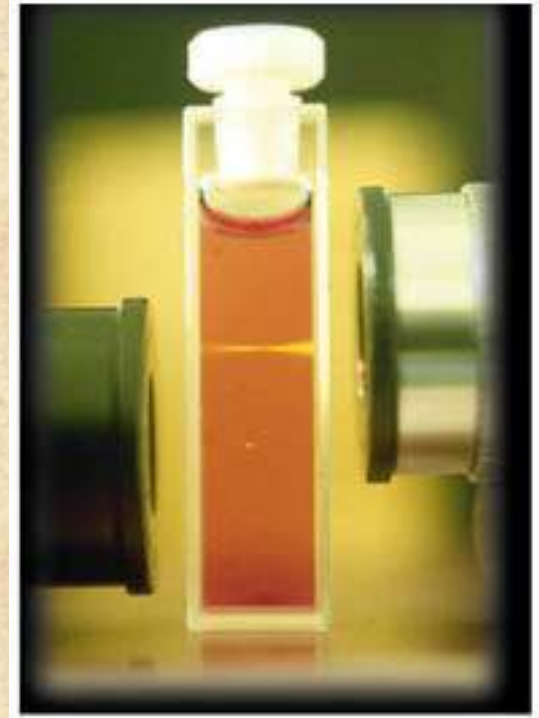
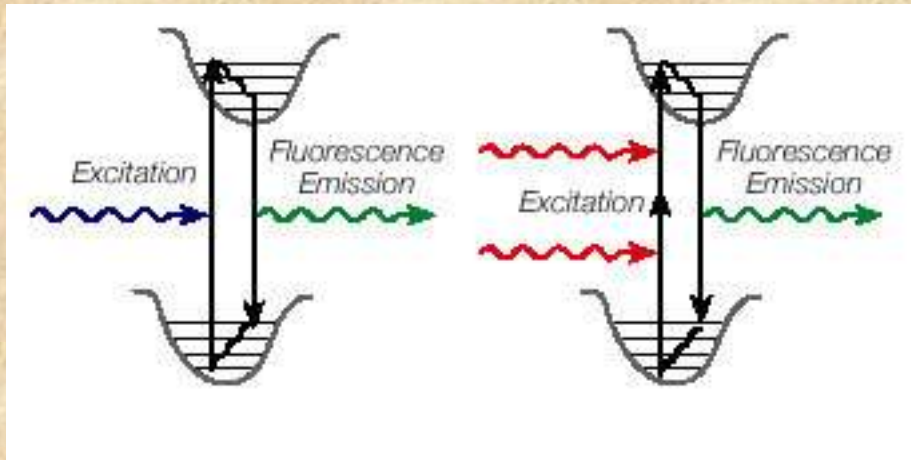
2 - Photon



Approximately $1 \mu\text{m}^3$

Defined by the wavelength
and numerical aperture of
the objective





Brad Amos
MRC, Cambridge, UK

Advantages of two-photon excitation

3-D sectioning effect

Absence of photo bleaching in out of focus regions

Large separation of excitation and emission

No Raman from the solvent

Deep penetration in tissues

Single wavelength of excitation for many dyes

High polarization

Why confocal detection?

Molecules are small, why to observe a large volume?

- Enhance signal to background ratio
- Define a well-defined and reproducible volume

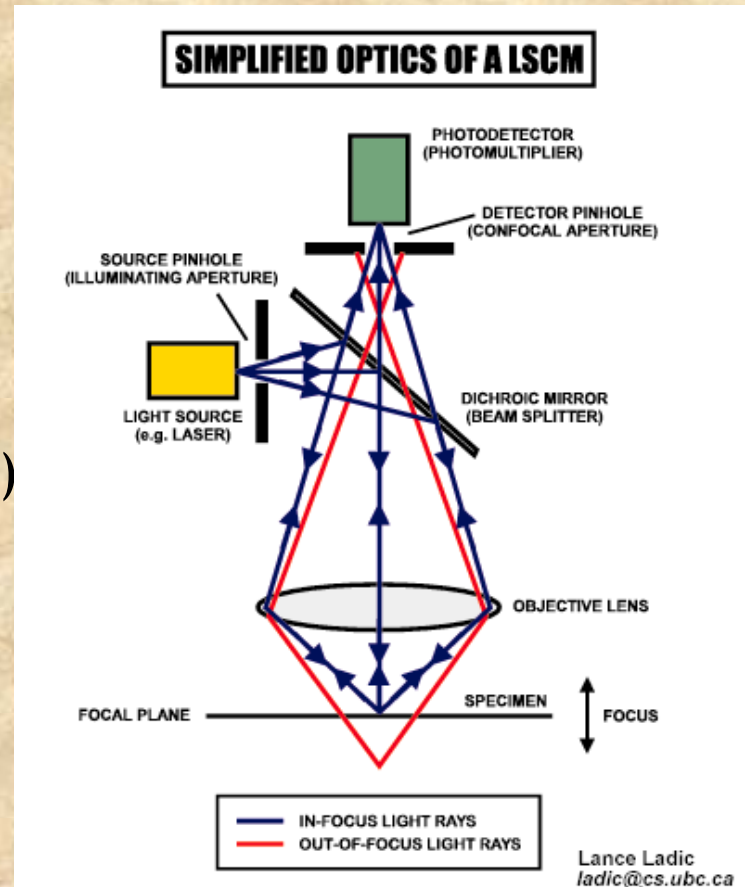
Methods to produce a confocal or small volume

(limited by the wavelength of light to about 0.1 fL)

- Confocal pinhole
- Multiphoton effects
 - 2-photon excitation (TPE)
 - Second-harmonic generation (SGH)
 - Stimulated emission
 - Four-way mixing (CARS)

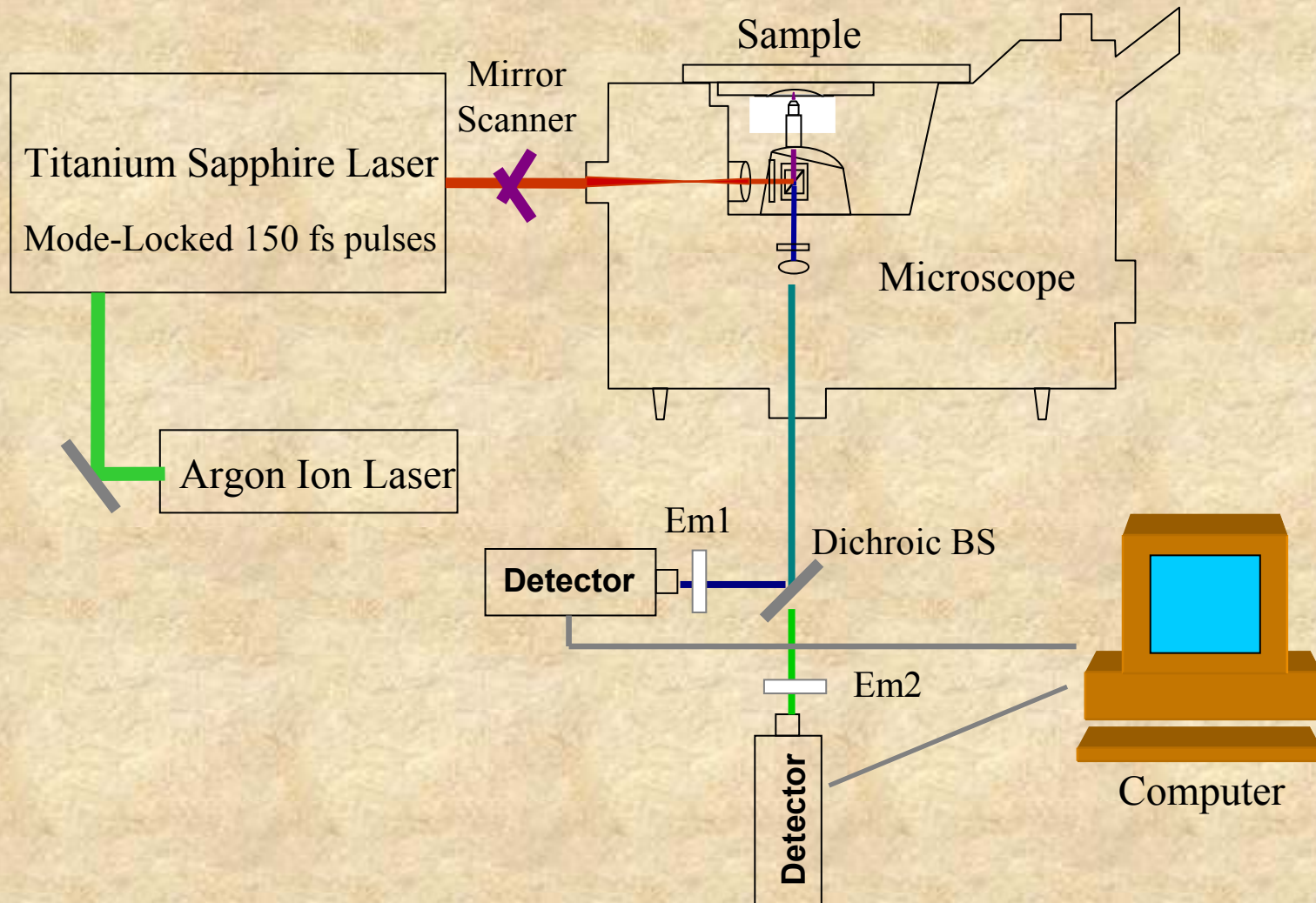
(not limited by light, not applicable to cells)

- Nanofabrication
- Local field enhancement
- Near-field effects



How does one create an observation volume and collect the data?

Two-Photon, Scanning, FCS Microscope



Laser technology needed for two-photon excitation

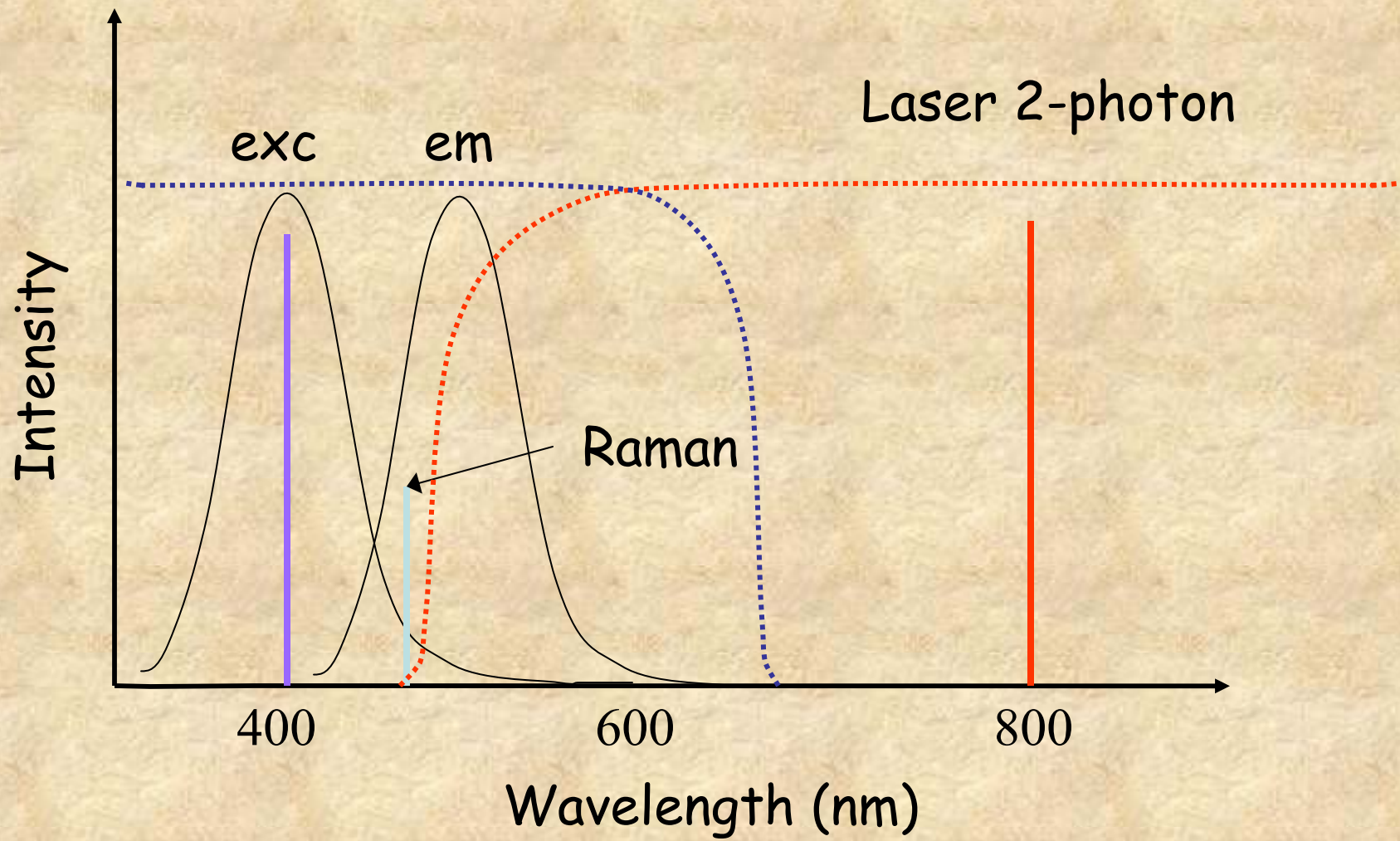
Ti:Sapphire lasers have pulse duration of about 100 fs
Average power is about 1 W at 80 MHz repetition rate
About 12.5 nJ per pulse (about 125 kW peak-power)
Two-photon cross sections are typically about

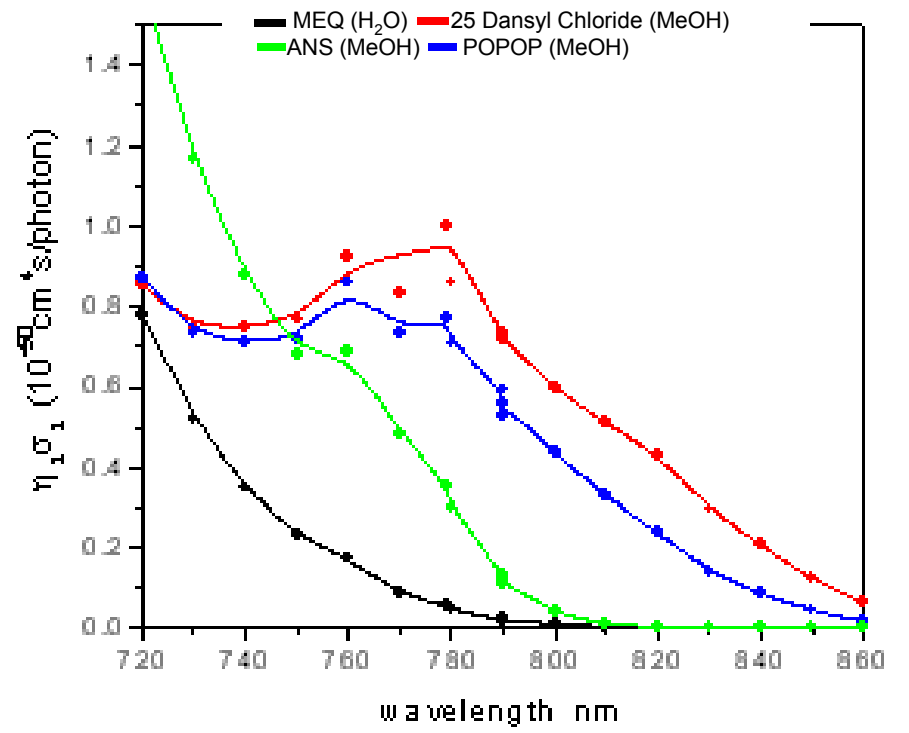
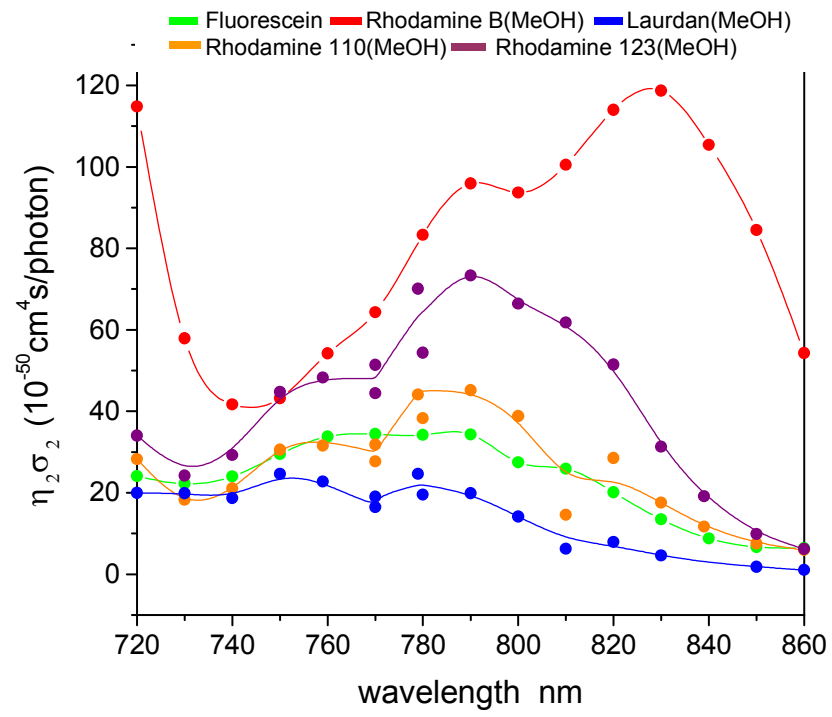
$$\delta = 10^{-50} \text{ cm}^4 \text{ sec photon}^{-1} \text{ molecule}^{-1}$$

Enough power to saturate absorption in a diffraction limited spot

$$n_a \approx \frac{d}{\tau} \left(\frac{p \pi A^2}{f h c \lambda} \right)^2$$

- n_a Photon pairs absorbed per laser pulse
- p Average power
- τ pulse duration
- f laser repetition frequency
- A Numerical aperture
- λ Laser wavelength
- d cross-section





General References

- Salmon, E. D. and J. C. Canman. 1998. Proper Alignment and Adjustment of the Light Microscope. Current Protocols in Cell Biology 4.1.1-4.1.26, John Wiley and Sons, N.Y.
- Murphy, D. 2001. Fundamentals of Light Microscopy and Electronic Imaging. Wiley-Liss, N.Y.
- Keller, H.E. 1995. Objective lenses for confocal microscopy. In “Handbook of biological confocal microscopy”, J.B.Pawley ed. , Plenum Press, N.Y.

On line resource:

Molecular Expressions, a Microscope
Primer at:

[http://www.microscopy.fsu.edu/primer/
index.html](http://www.microscopy.fsu.edu/primer/index.html)